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Methodology of Magnetic Resonance Spectroscopy: MRS



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Welcome to New Haven



Overview

What is MRS?

What is Spectroscopic Imaging?



What is Image Segmentation?

What is ^{13}C MRS?

Overview

What is MRS?

What is Spectroscopic Imaging?

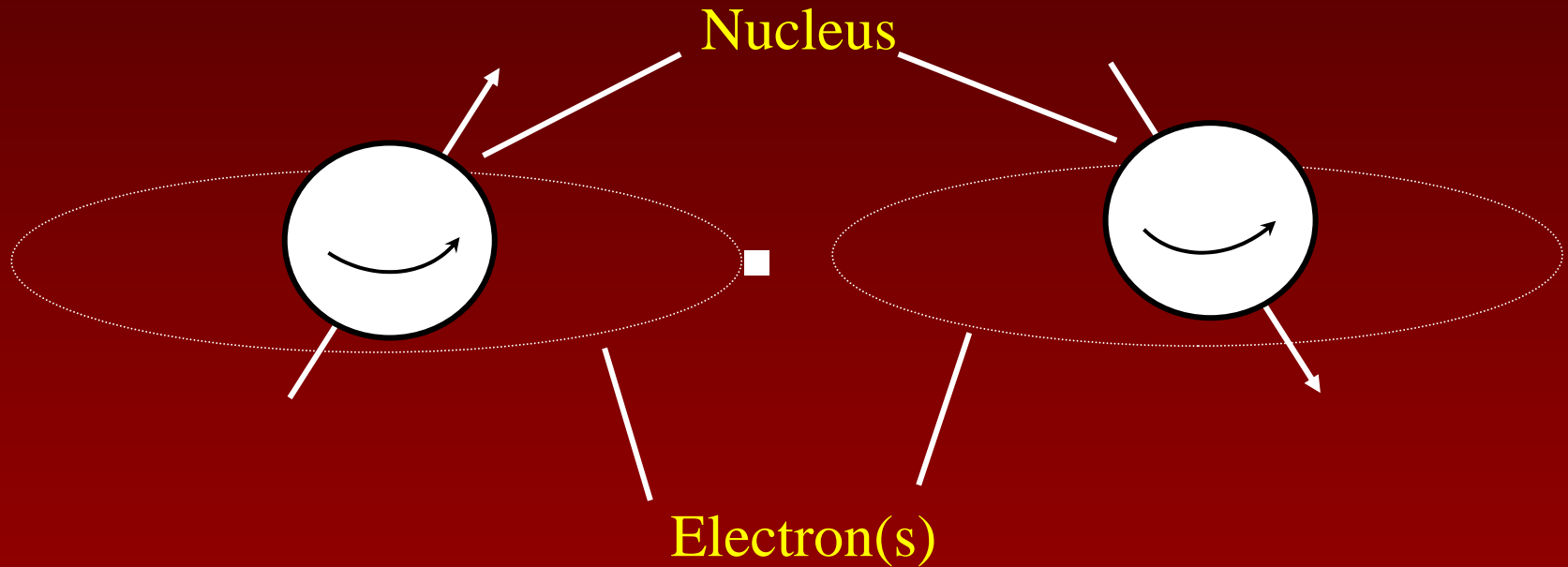


What is Image Segmentation?

What is ^{13}C MRS?

Methods: What is MRS?

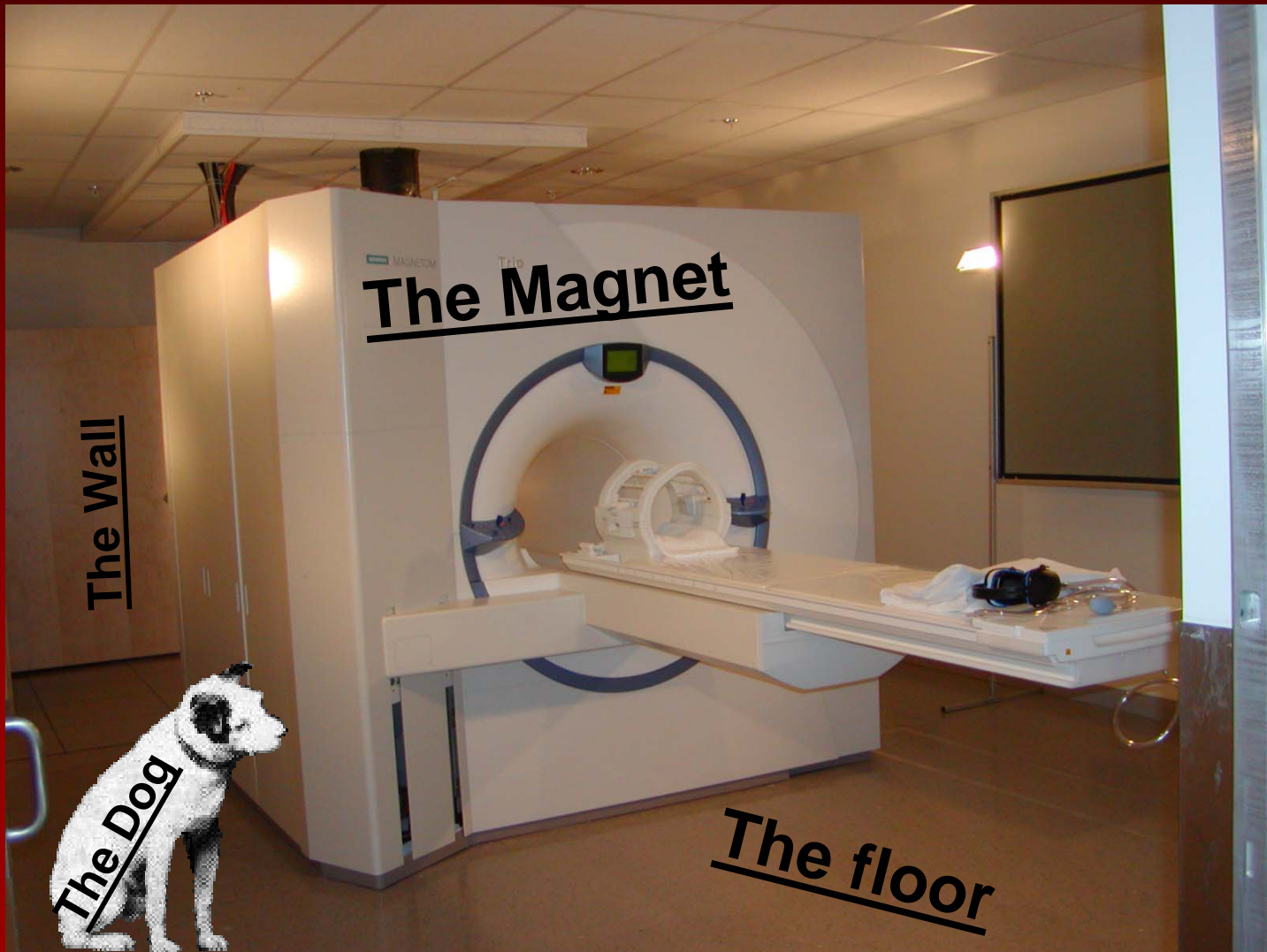
Nuclear Magnetic Resonance Spectroscopy



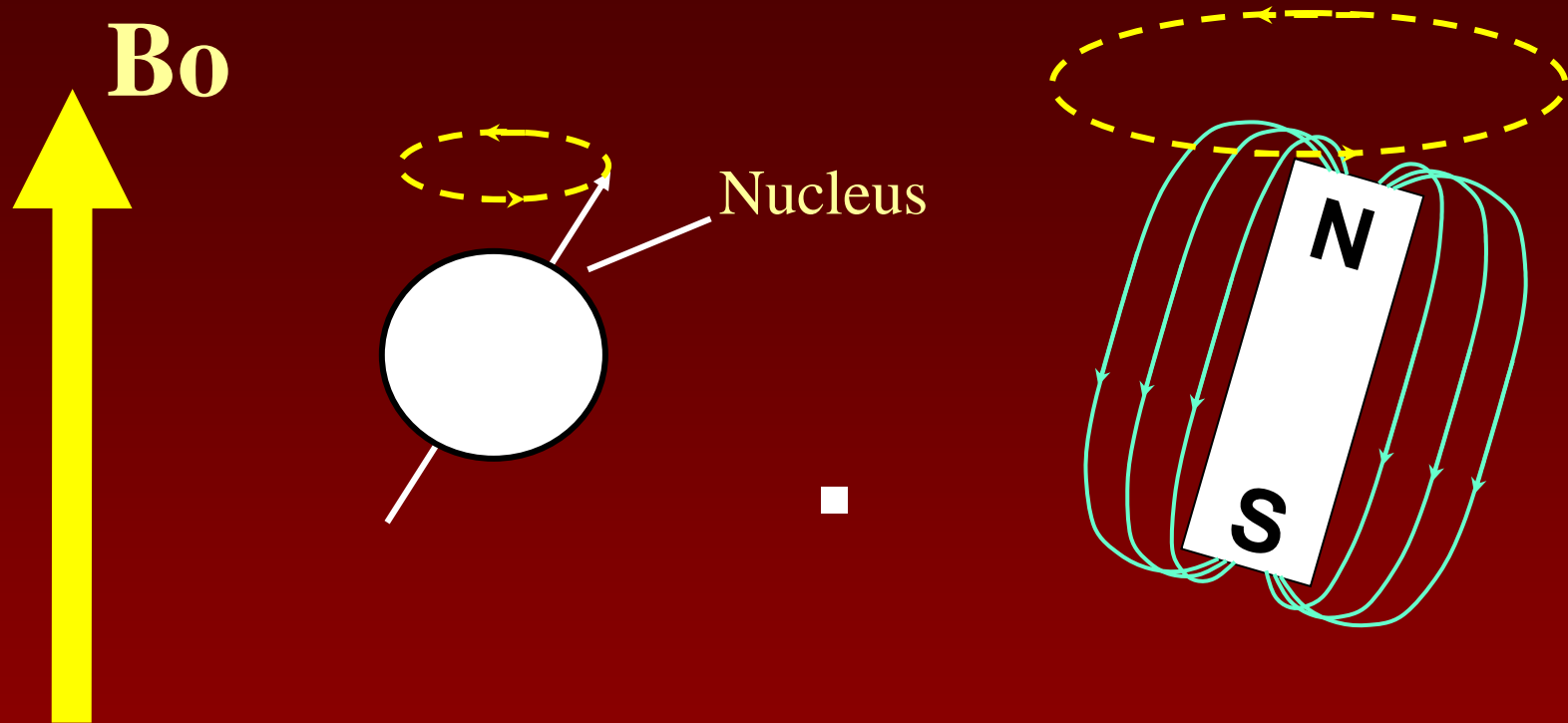
Spin of nucleus is either 'up' or 'down'.

Methods: What is MRS?

Subject lies inside a large magnet to orient the spins.



Rotating Magnetic Dipole



In a large magnetic field (scanner magnet), the magnetic dipole precesses about the axis of the large field with a frequency $\nu = \gamma B_0 / 2\pi$.

Only nuclei with *spin* can be detected with MRS.

Some NMR-Visible Nuclei

^1H – water, lipids, amino acids, many other metabolites

$$\gamma = 2.67 \times 10^4 \text{ radians/sec/Gauss}$$

^{13}C - amino acids, neurotransmitters, glucose, lipids, acetate

$$\gamma = 0.67 \times 10^4 \text{ radians/sec/Gauss}$$

^{15}N - metabolism of ammonia, amino acids

^{19}F - pharmacokinetics of fluoxetine and fluvoxamine

^{23}Na - effects of hypoxia, challenges to Na pumps

^2H - metabolism of fats

^7Li - pharmacokinetics of lithium

Transition from Quantum to Classical Mechanics

1.5 mM GABA, 13.5 cc voxel
contains 2.4×10^{22} hydrogen nuclei
for GABA detection

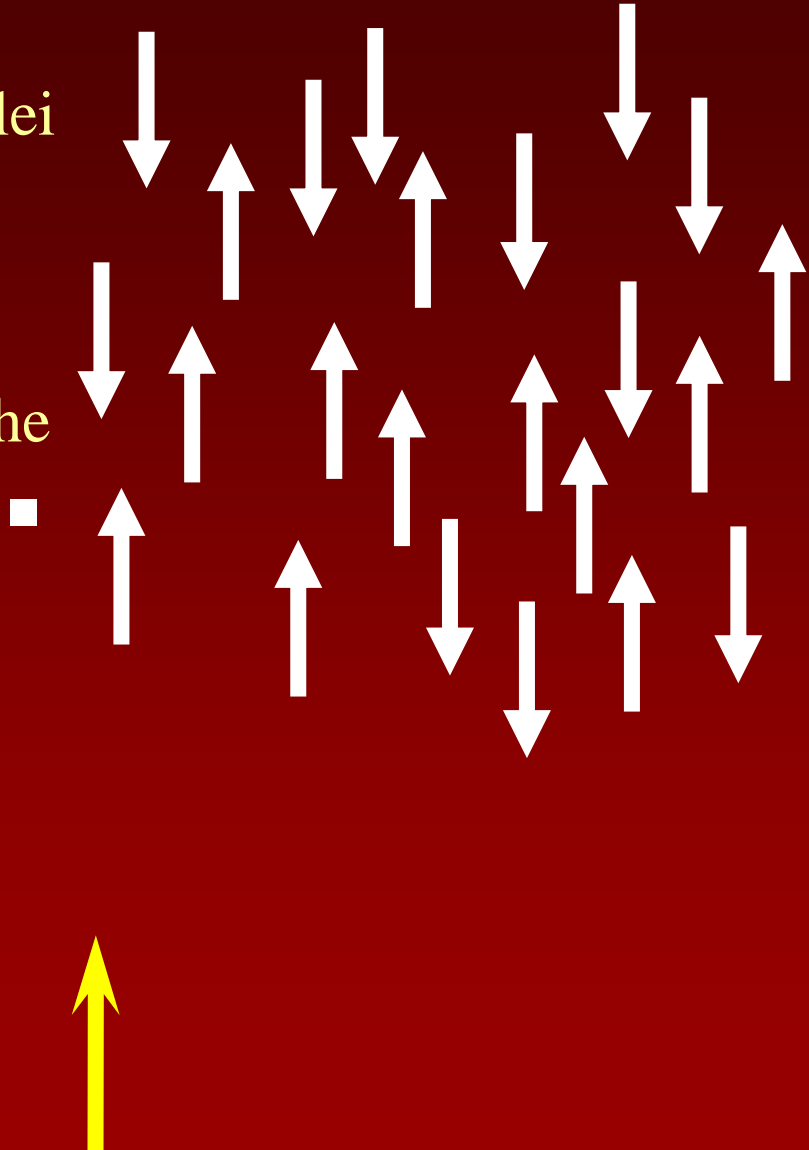
The large number of particles
allows a meaningful analysis of the
behavior of the whole group.

Boltzmann distribution:
$$N_+/N_- = \exp(-\gamma\hbar B_0/2\pi kT)$$

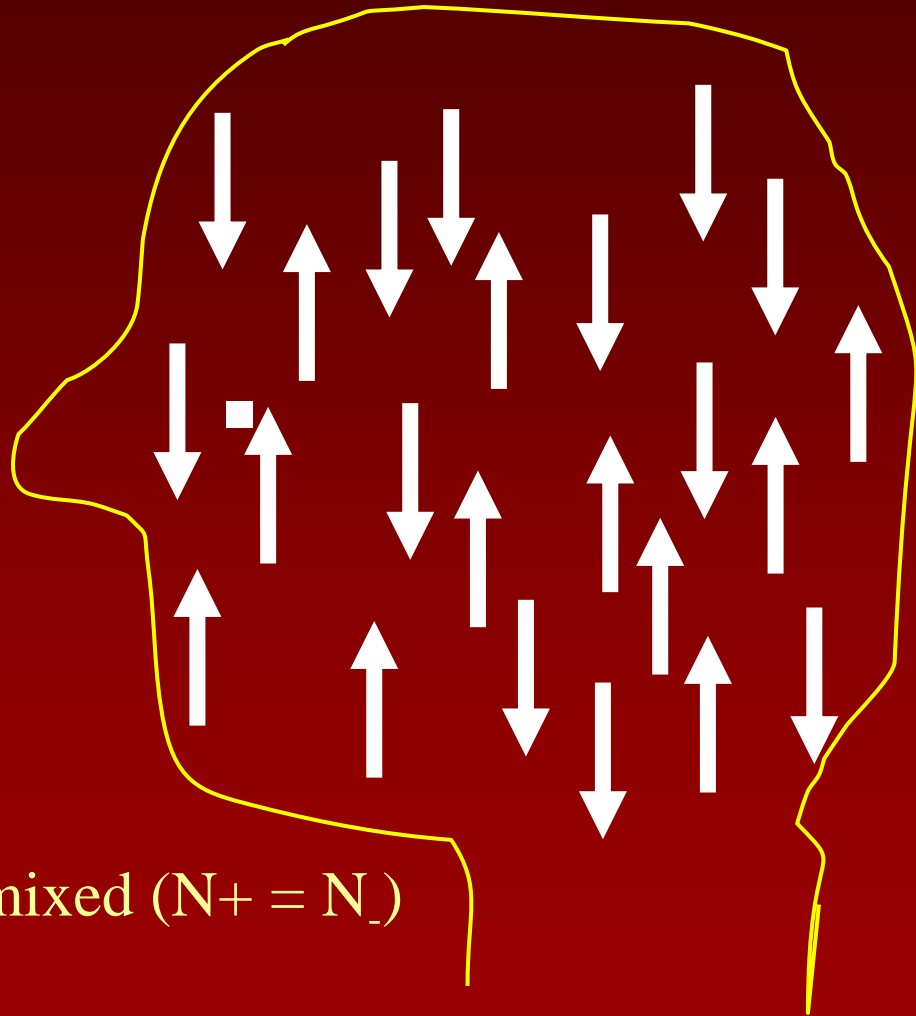
approximated as

$$N_+/N_- = 1 - \gamma\hbar B_0/2\pi kT$$

N_+ minus N_- is the net magnetization:

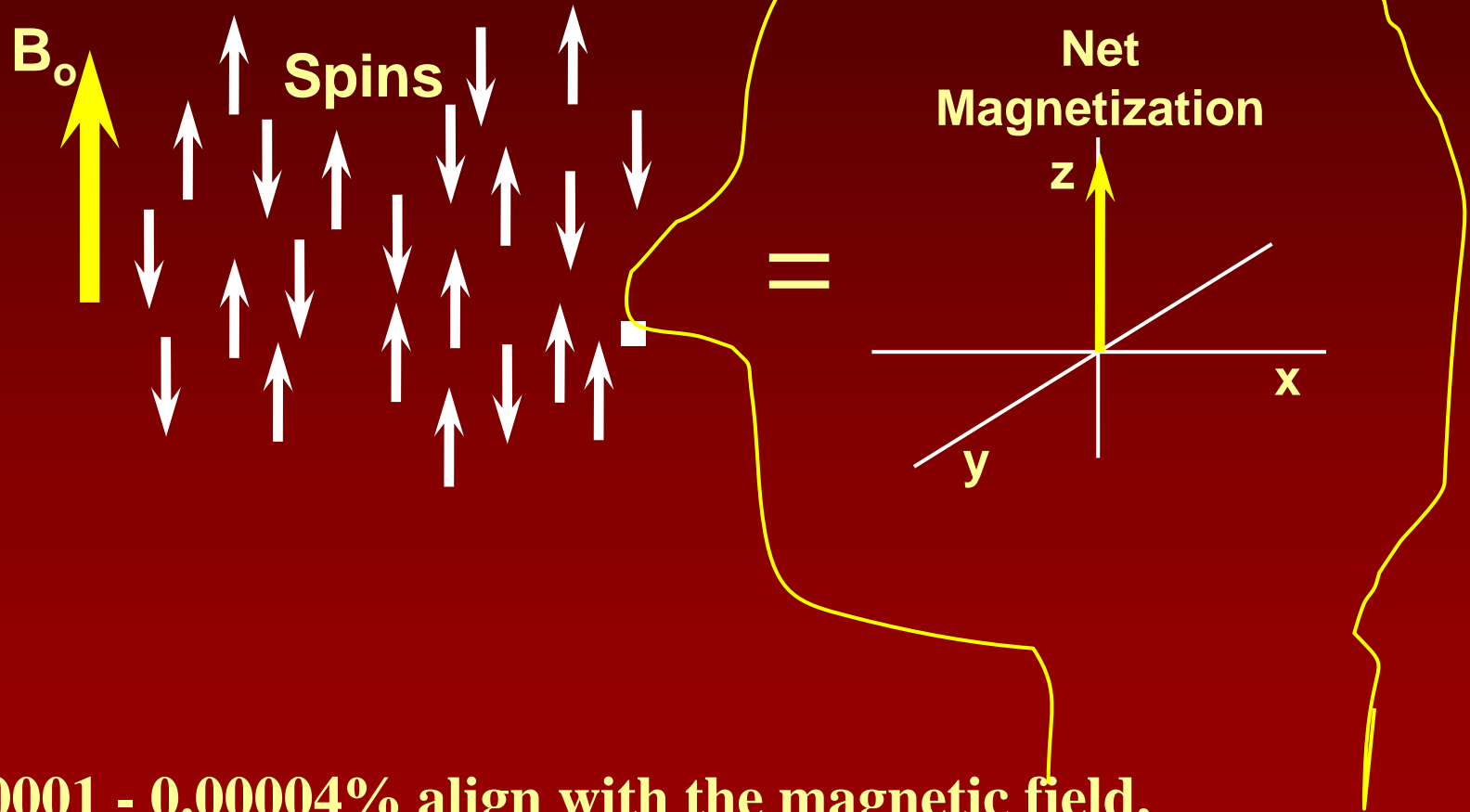


Spin Orientation in a Head (Outside the Scanner)



Spins evenly mixed ($N_+ = N_-$)

Inside Scanner (Strong Magnetic Field)



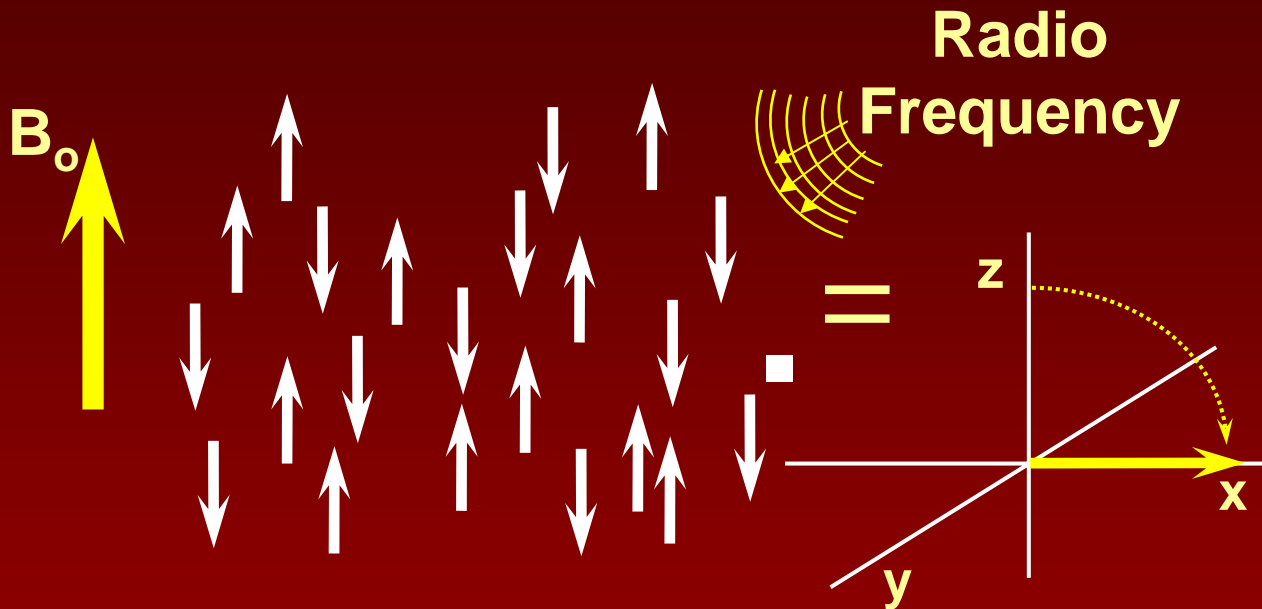
**0.00001 - 0.00004% align with the magnetic field,
creating net magnetization in the head.**

What is MRS?

Subject lies inside a large magnet to orient the spins.

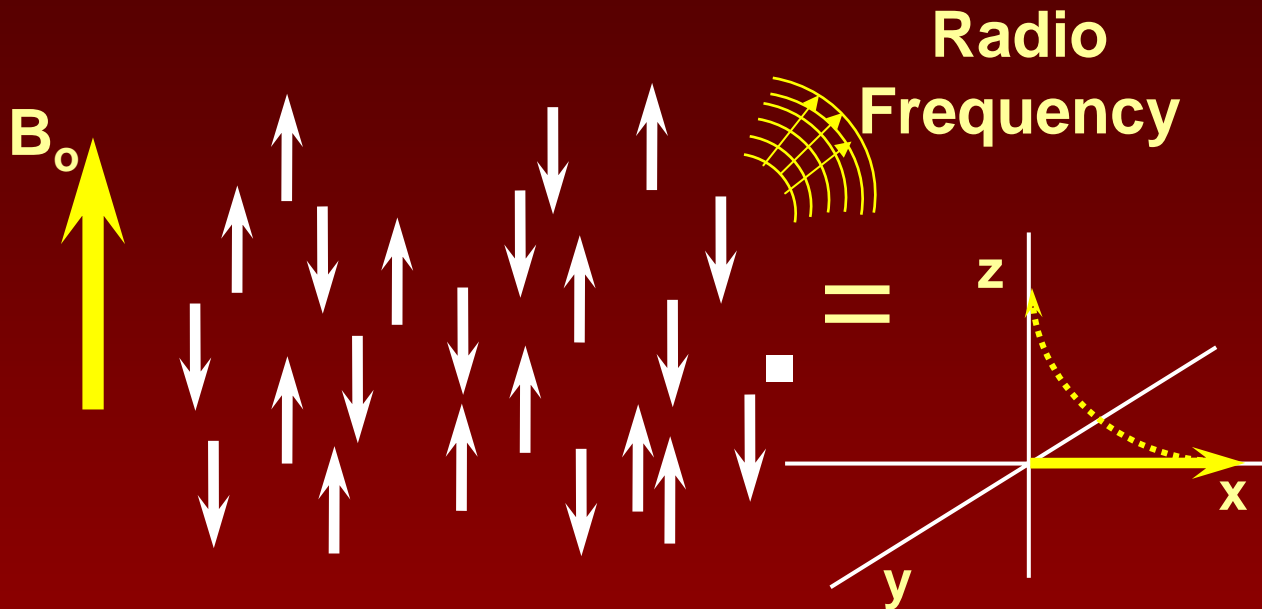


Radio Frequency Energy Applied



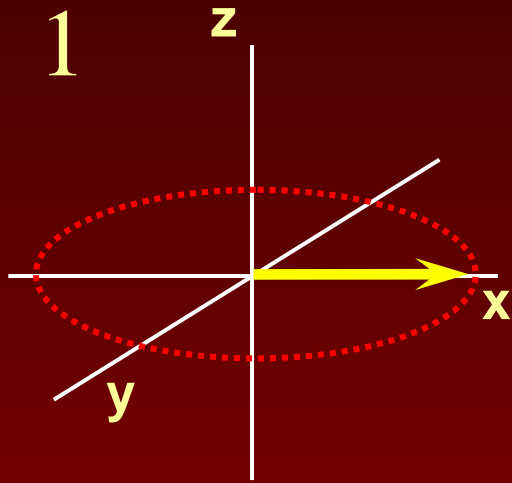
The net magnetization is altered by the application of energy at the proper frequency.

Longitudinal (T_1) Relaxation

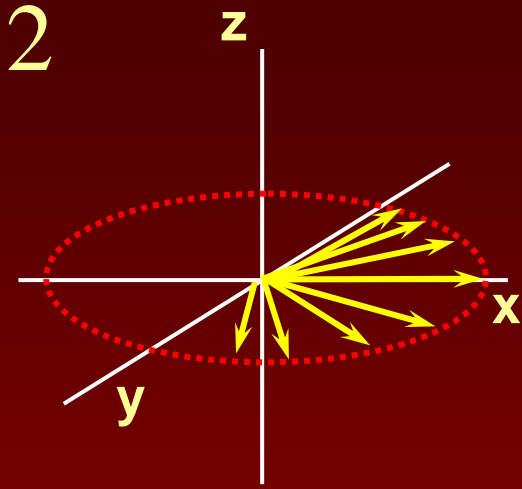


The magnetization returns to its original orientation at a rate governed by the exponential constant T_1 .

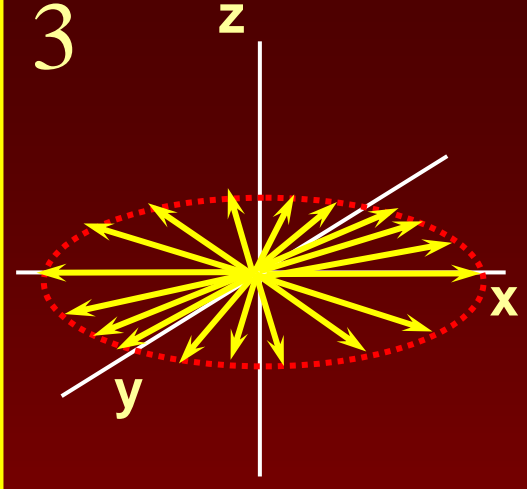
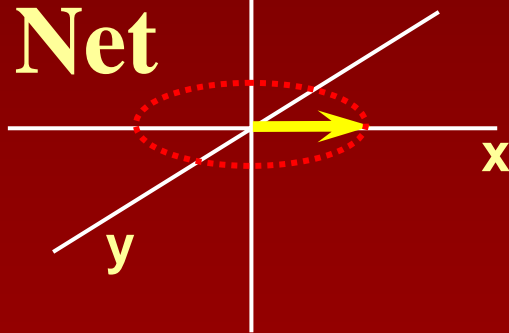
Transverse (T_2) Relaxation



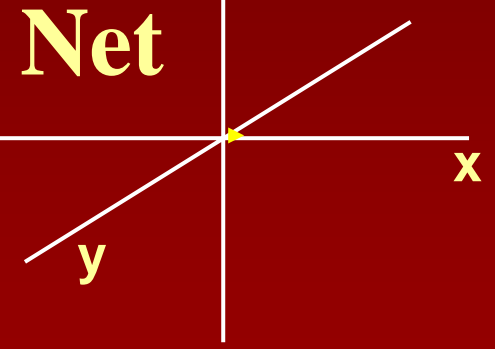
SIGNAL



SIGNAL



SIGNAL



Phase coherence is lost as the spins dephase due to microscopic magnetic field inhomogeneity.

MRS Frequencies Distinguish Chemicals: Sources of Differences in NMR Frequencies

1. Nucleus and Magnetic Field Strength (MHz)

Nucleus:

Example: ^{13}C frequency $\approx 25\%$ ^1H frequency

Magnetic Field Strength:

For ^1H , $42.6\text{MHz} \times \text{field strength (Tesla)}$

Examples:

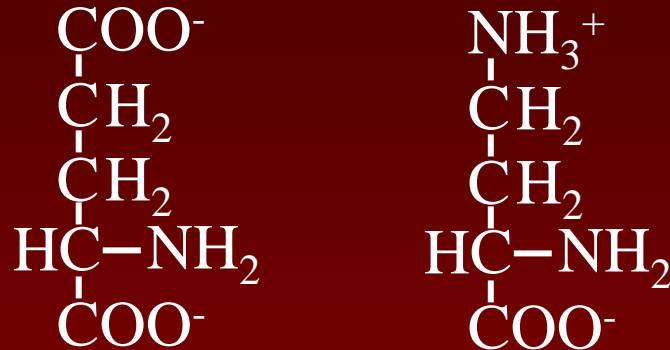
a. $1.5\text{T} = 63.9 \text{ MHz}$

b. $2.1\text{T} = 89.4 \text{ MHz}$ (~public radio - Bridgeport)

c. $4 \text{ T} = 170 \text{ MHz}$

Sources of Differences in NMR Frequencies

2. Molecular identity (Hz to thousands of Hz)



Glutamate

Glutamine

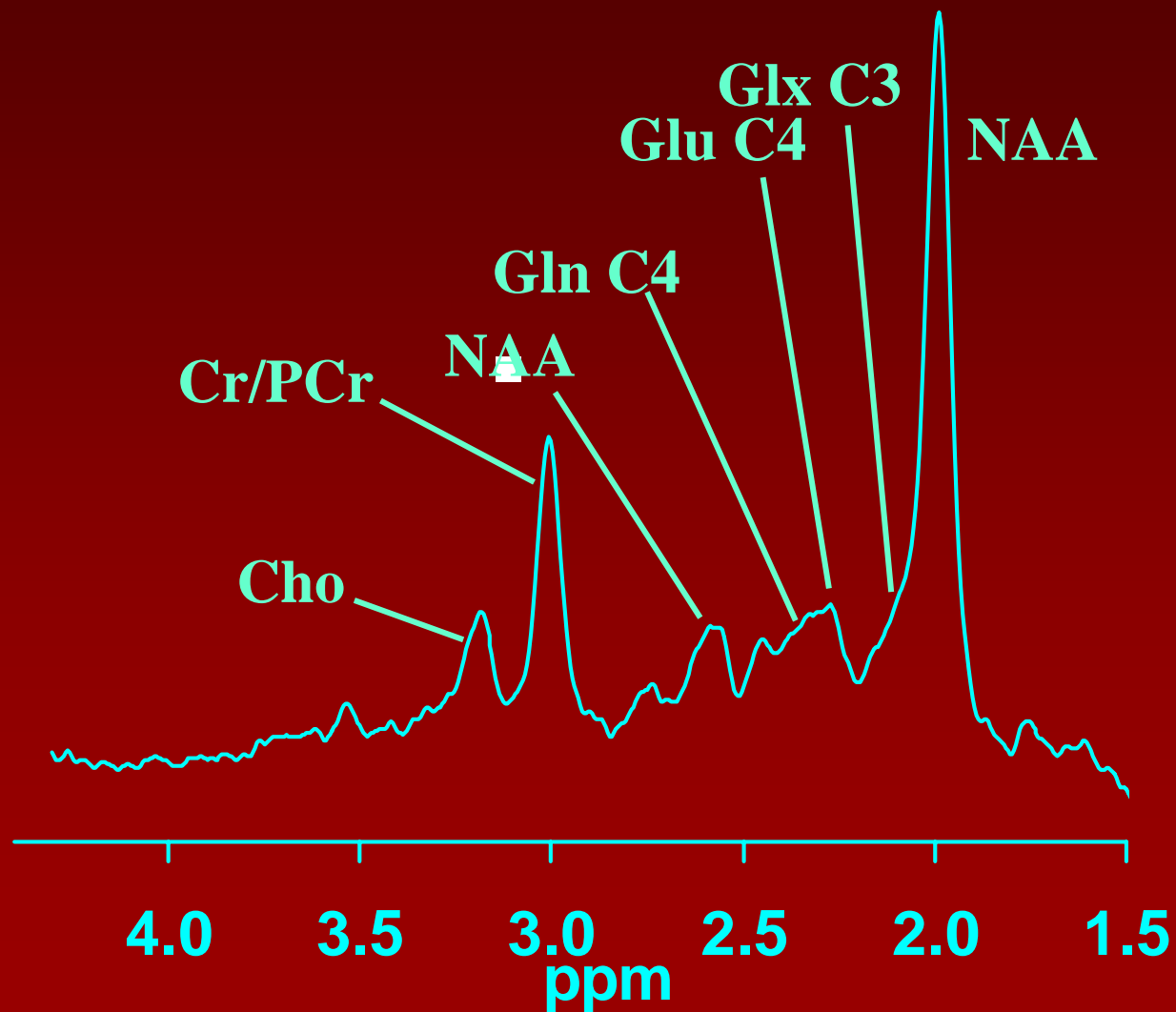
- Different molecules respond with slightly different frequencies.

- At 2.1T, glutamate responds at 89,633,931 Hz
glutamine responds at 89,633,940 Hz

3. J-coupling: (Hz to hundreds of Hz) (used for GABA editing)

MRS

MRS of the human brain: chemicals separated by frequency



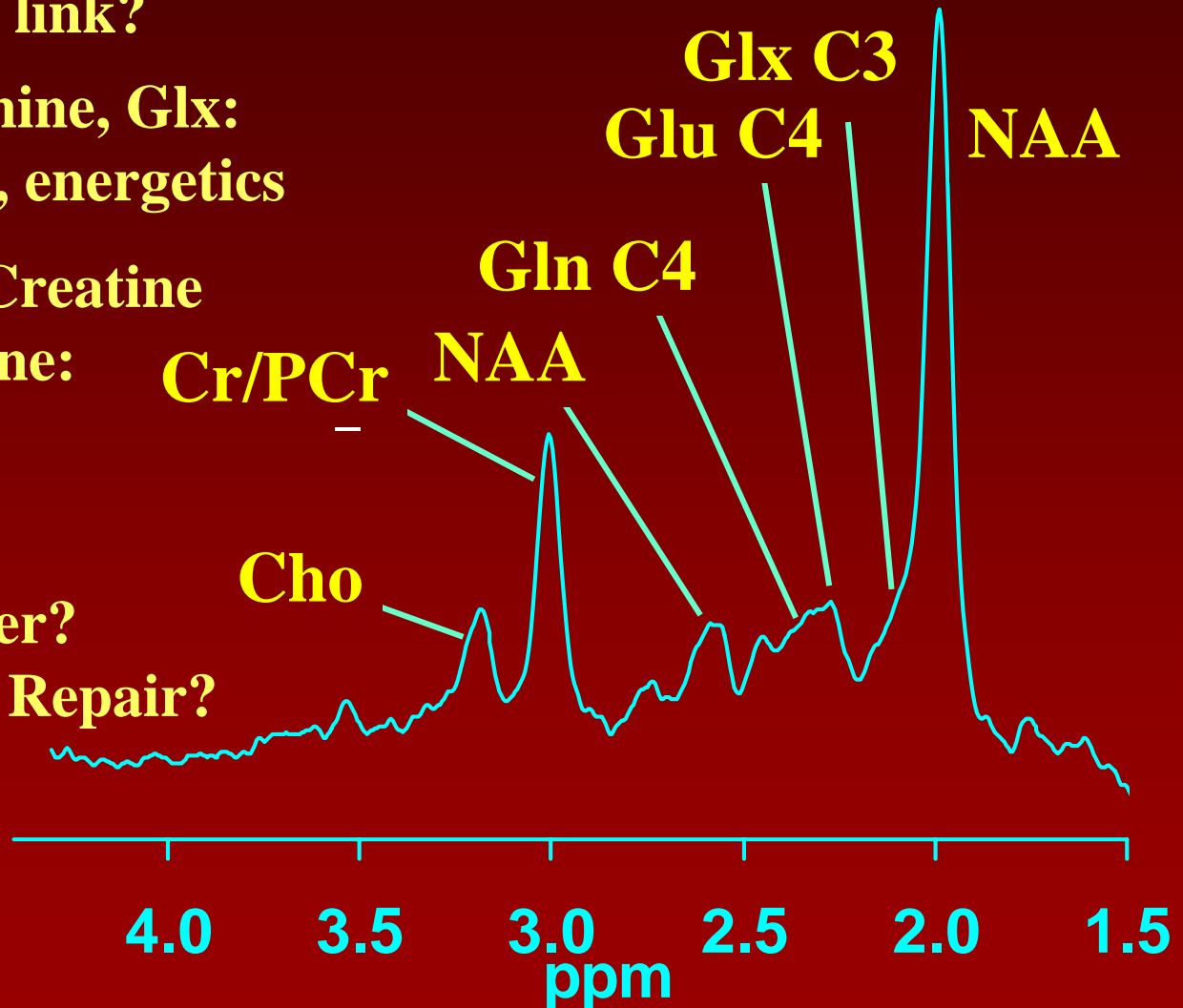
MRS: Significance

N-AcetylAspartate: neuronal viability, energetic link?

Glutamate, Glutamine, Glx: neurotransmission, energetics

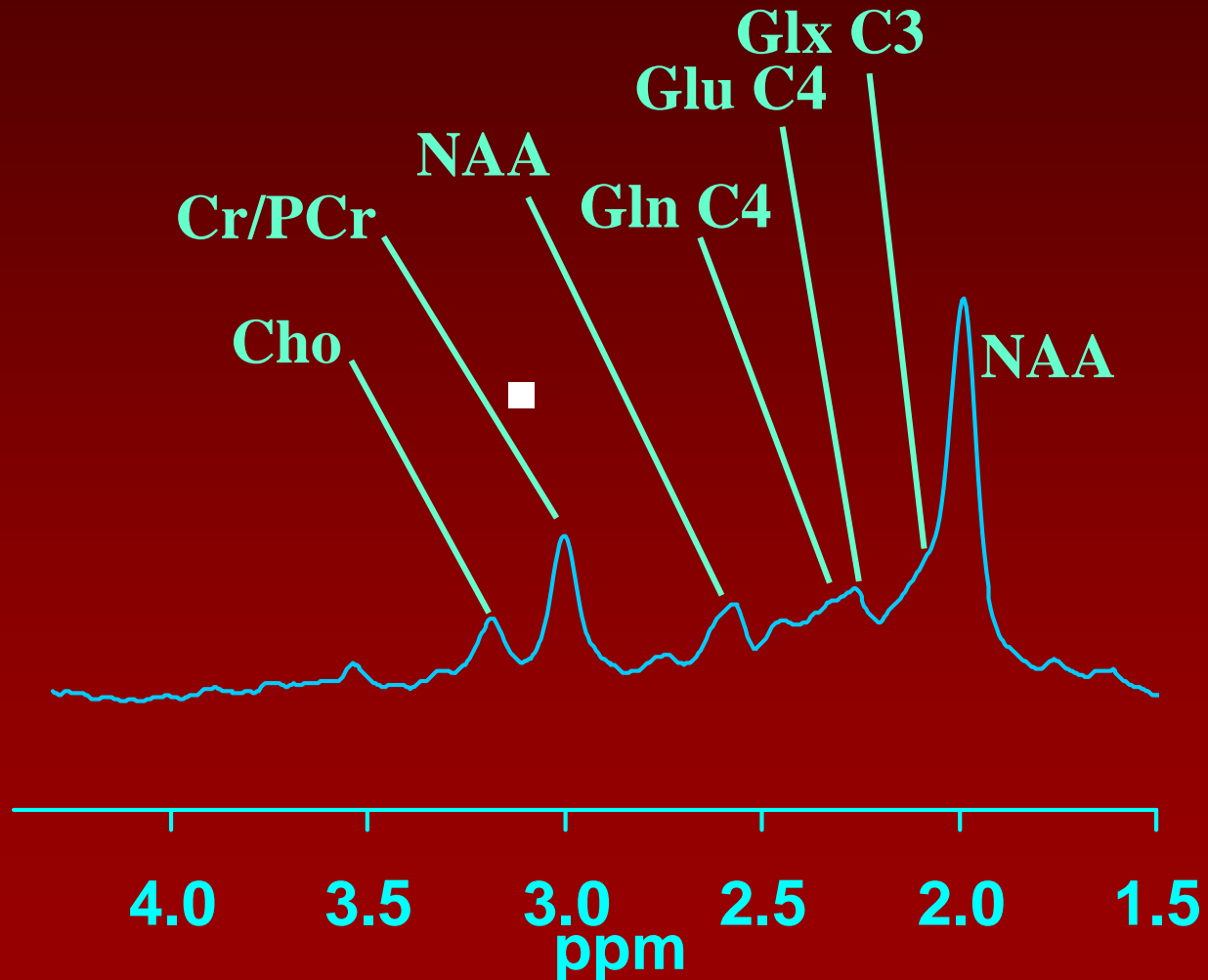
Cr/PCr: Total of Creatine and Phosphocreatine: Largely inert

Choline: Membrane Turnover? Cell Damage? Cell Repair?



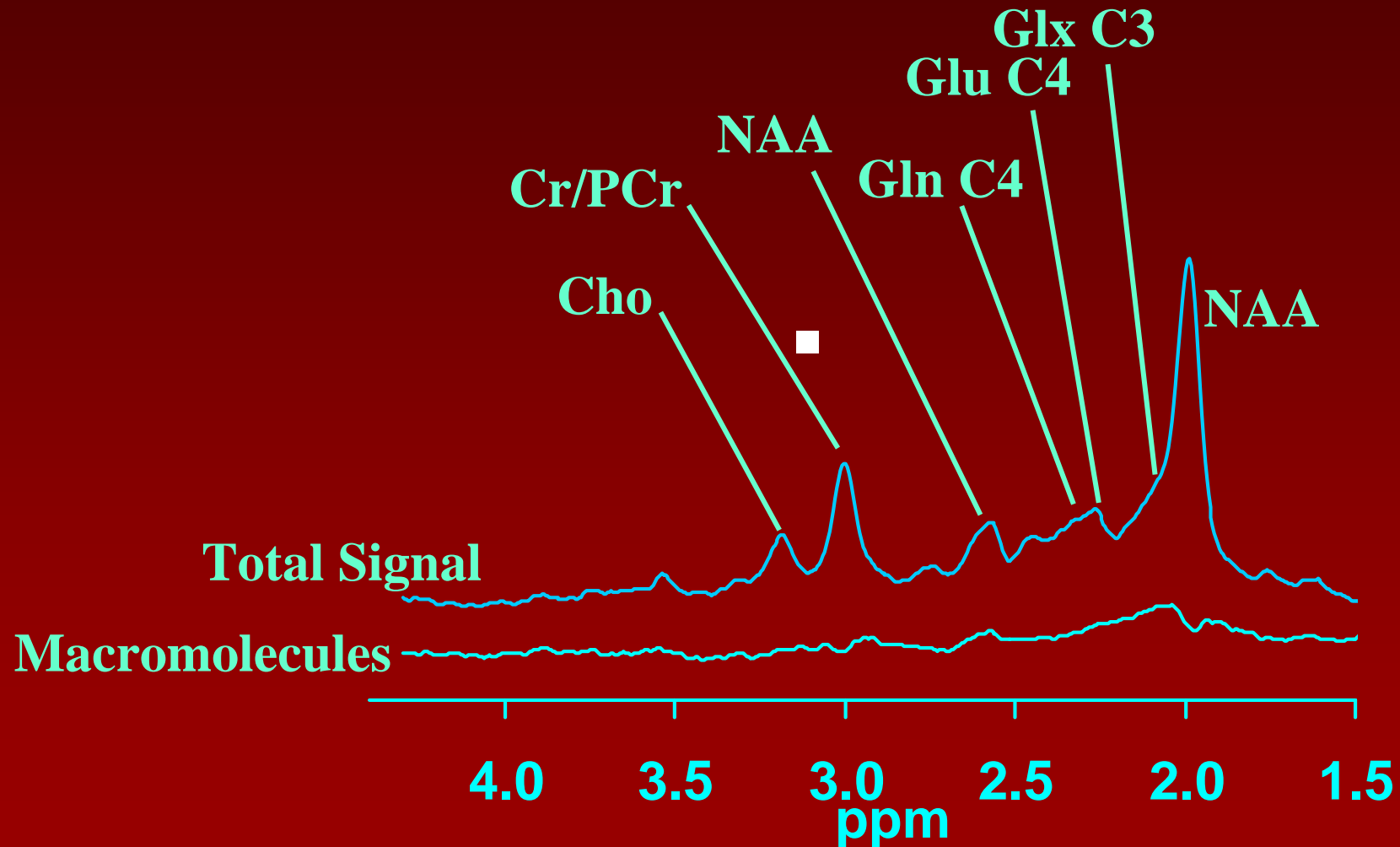
MRS

Short-echo measurement of glutamate, N-acetylaspartate, and other metabolite: **What else is present?**



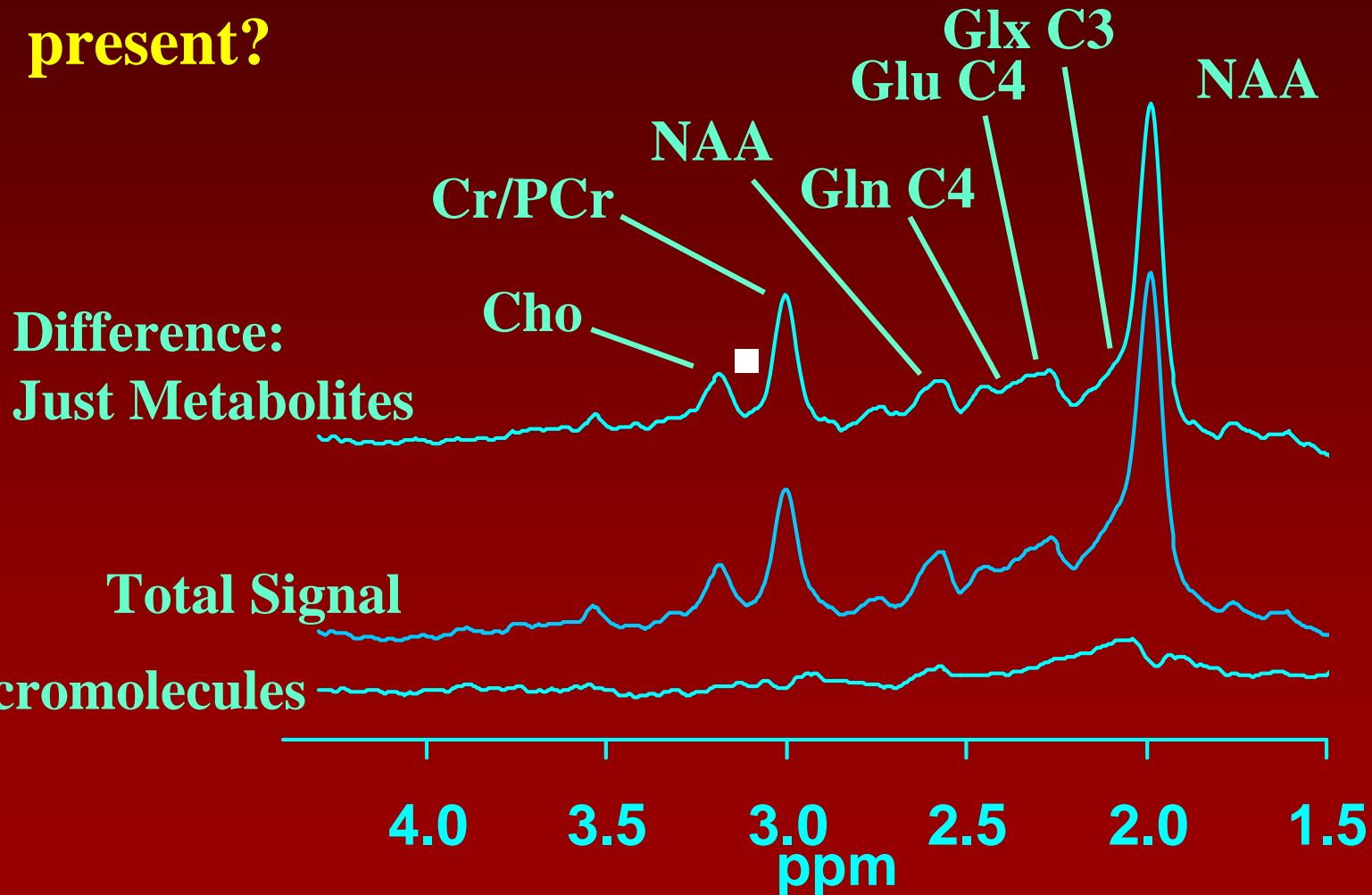
MRS

Short-echo measurement of glutamate, N-acetylaspartate, and other metabolite: Macromolecules in baseline



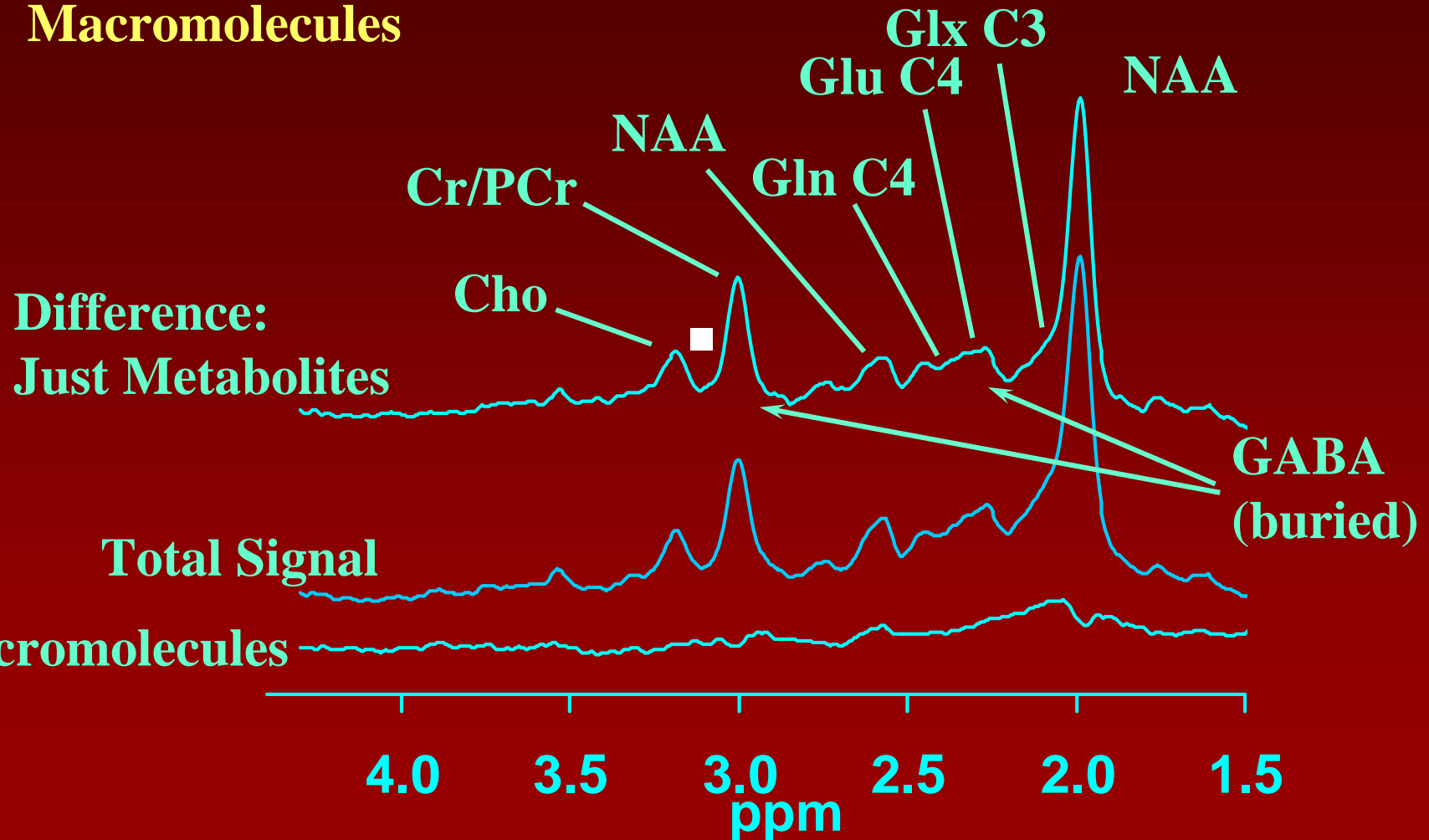
MRS

Short-echo measurement of glutamate, N-acetylaspartate, and other metabolite: Macromolecules out. **What else is present?**



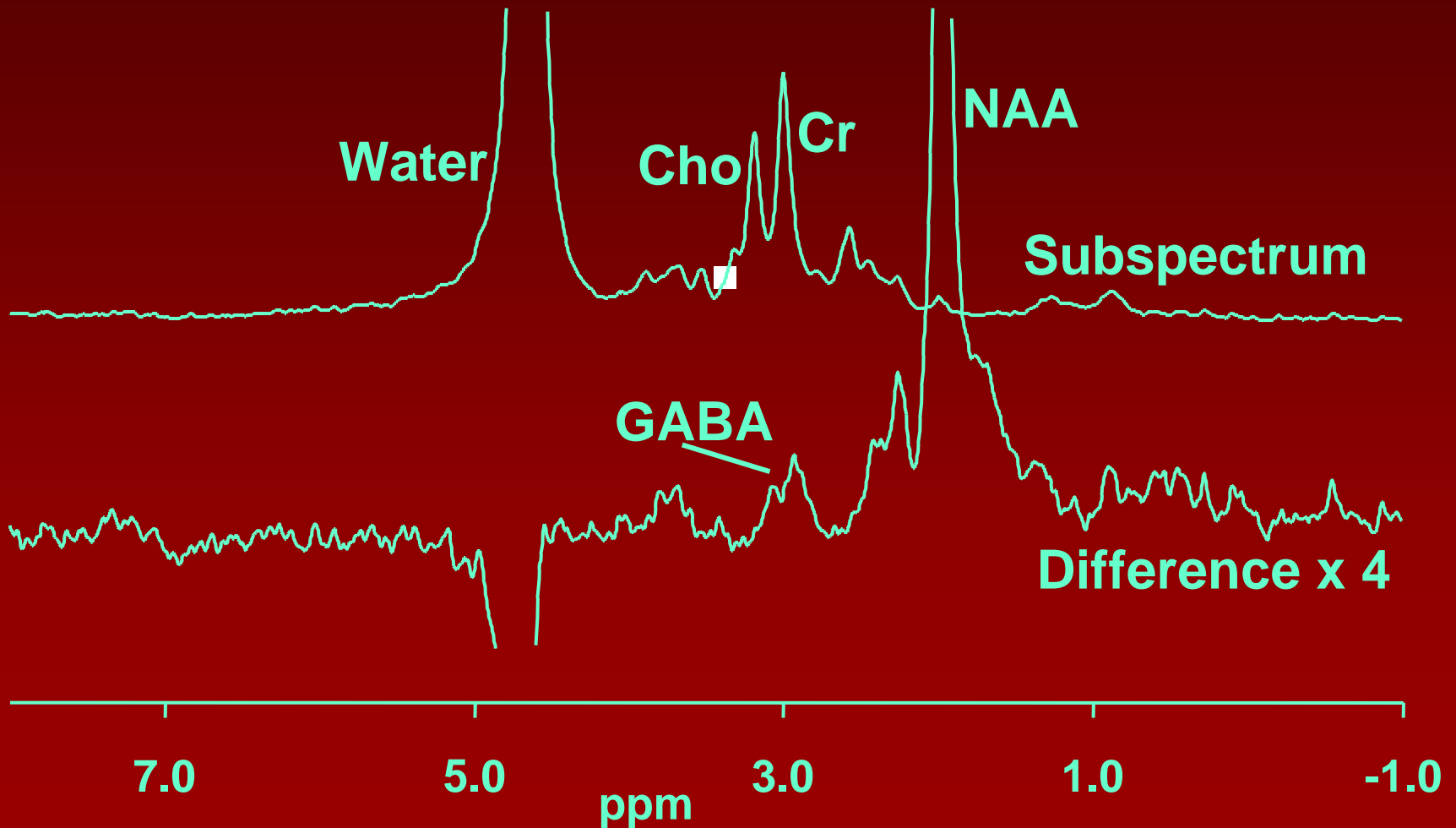
MRS

Short-echo measurement of glutamate, N-acetylaspartate, and other metabolite: Measurement and Removal of Macromolecules



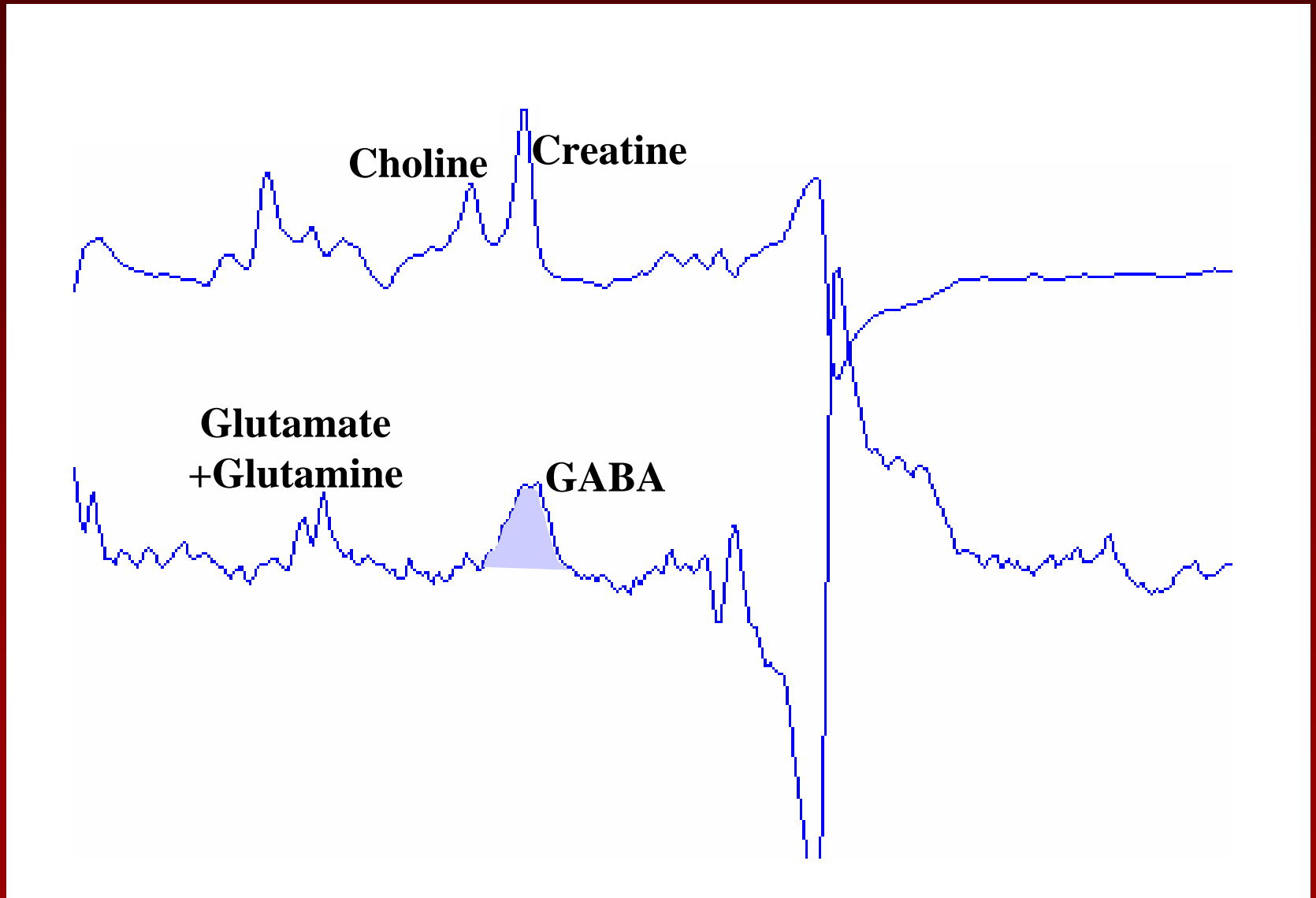
MRS

**^1H MRS measurement of GABA, Bruker 2.1T MR scanner,
13-22 cc occipital voxel: J-editing difference method**

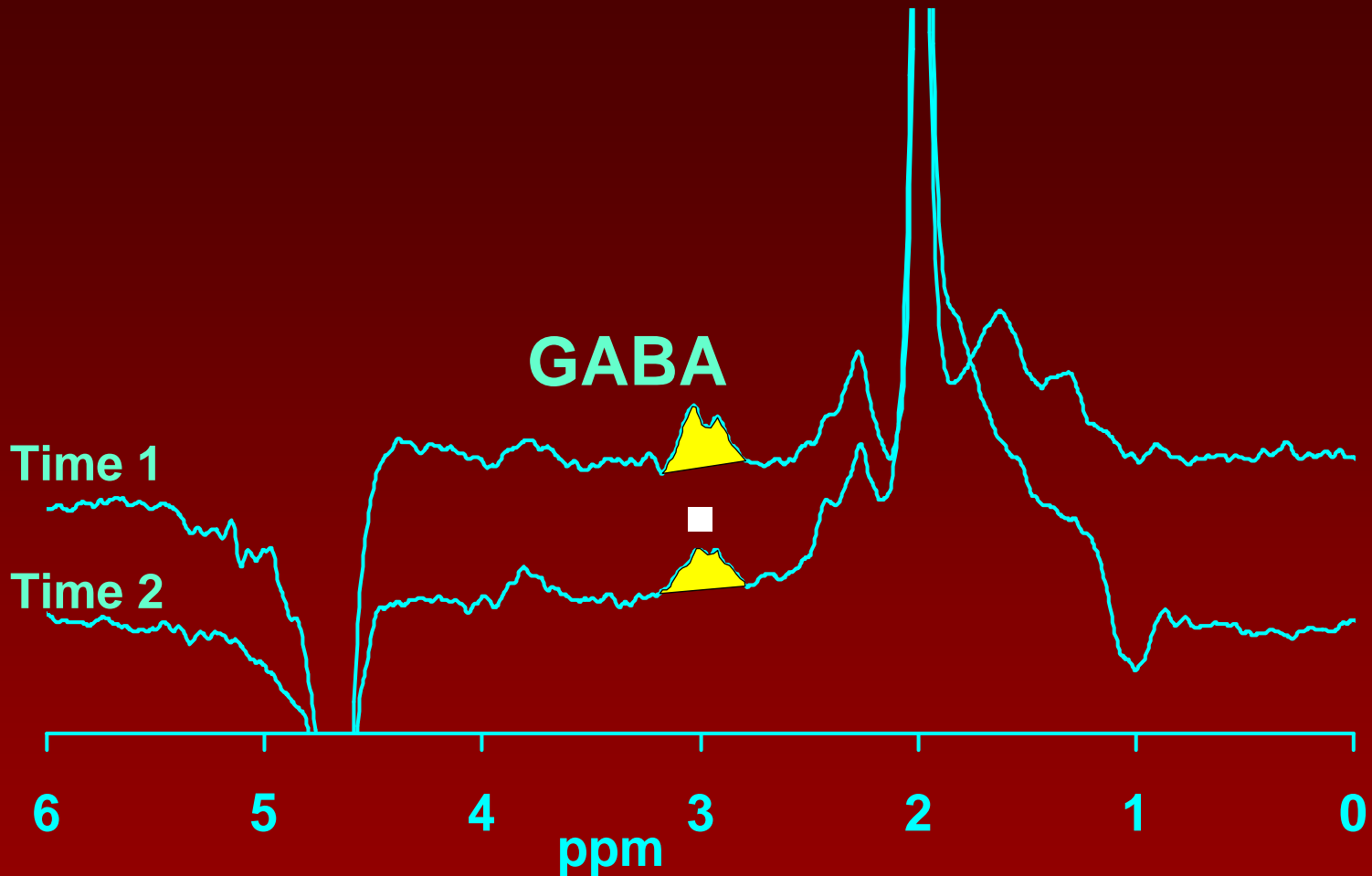


GABA Editing

•8 cc at 4T.

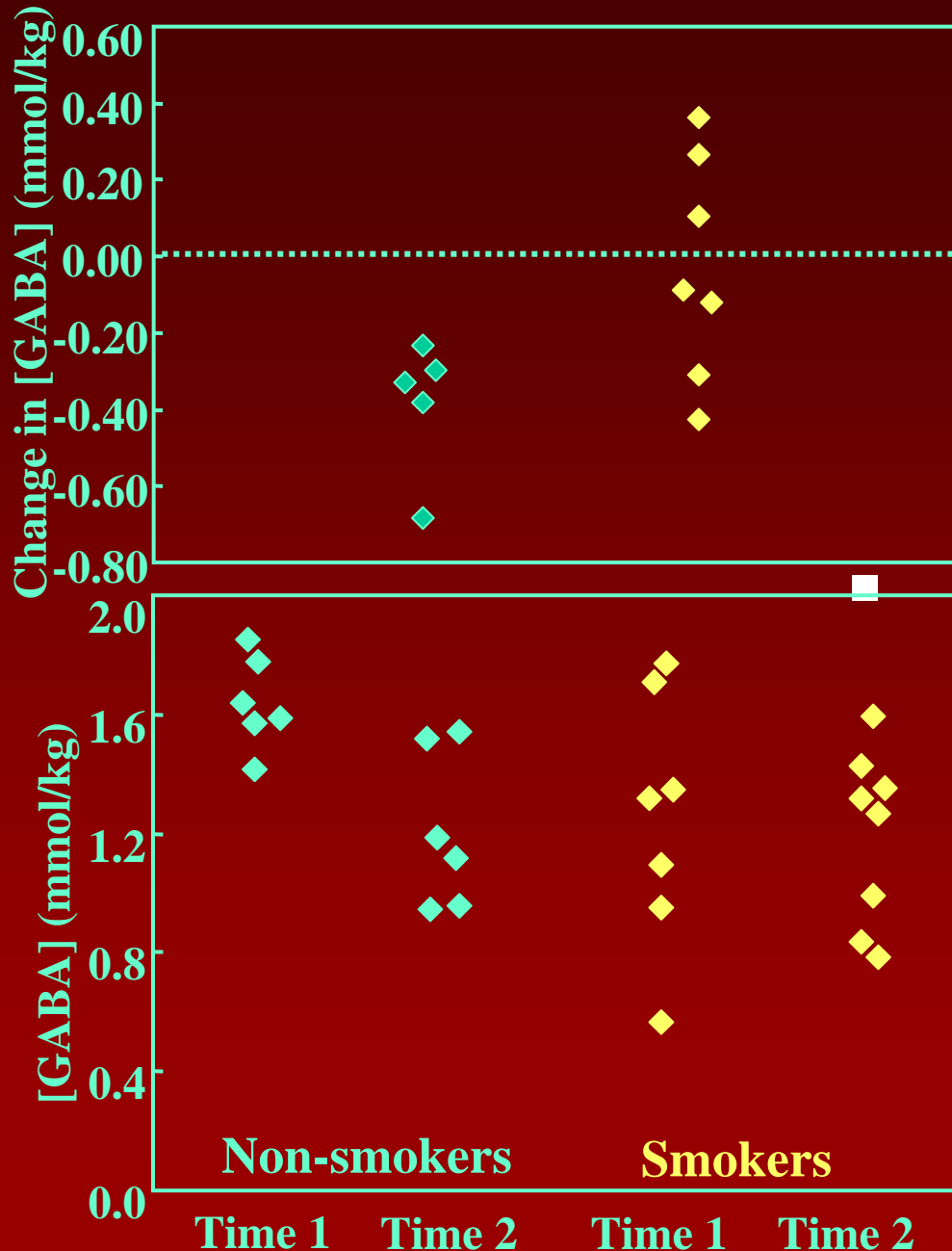


GABA in One Alcohol-Dependent Subject



Spectra of cortical GABA obtained in one subject at one week and one month of sobriety. GABA was reduced at one month.

Effects of 1 Month of Sobriety on GABA



- Changes in GABA levels with sobriety depended on smoking ($p = 0.03$).

- GABA in non-smokers fell by 0.39 ± 0.18 mmol/kg ($p = 0.004$), but GABA in smokers did not ($p = 0.75$).

- GABA in non-smokers at time 1 differed from the non-smokers' GABA at time 2 ($p = 0.03$).

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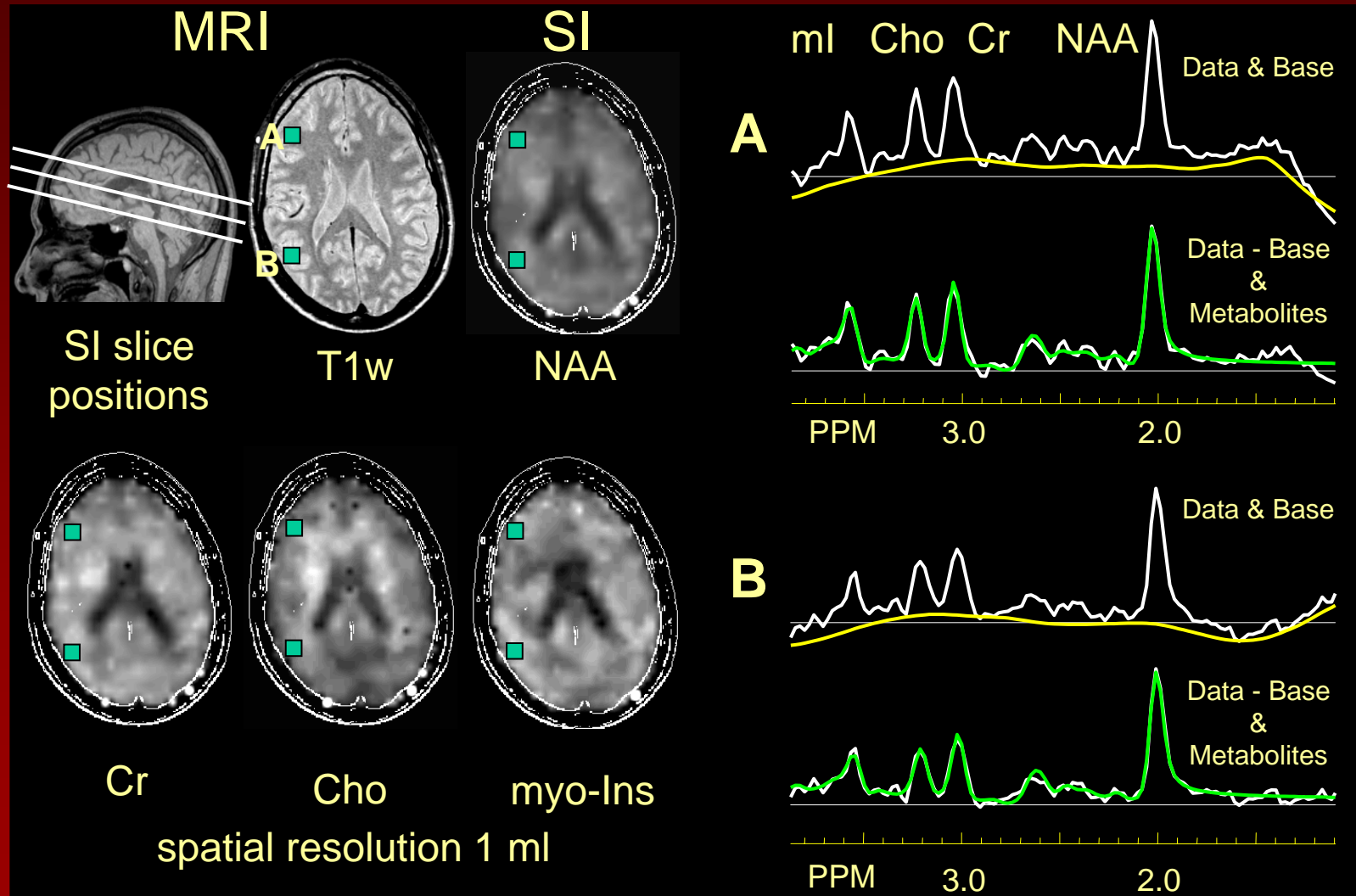


What is Image Segmentation?

What is ^{13}C MRS?

^1H MR Spectroscopic Imaging TE = 25 ms

Metabolite Distribution and Quantification



Overview

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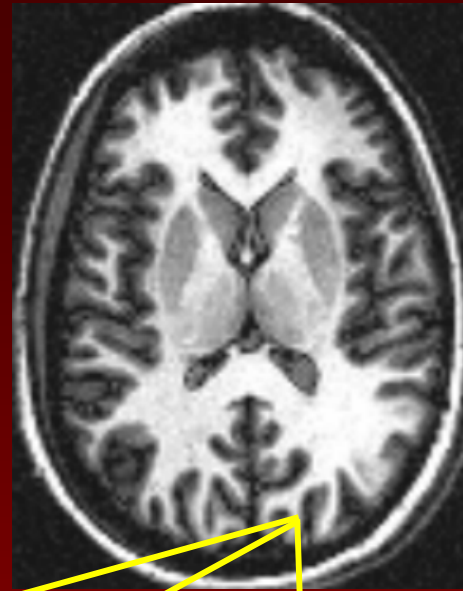


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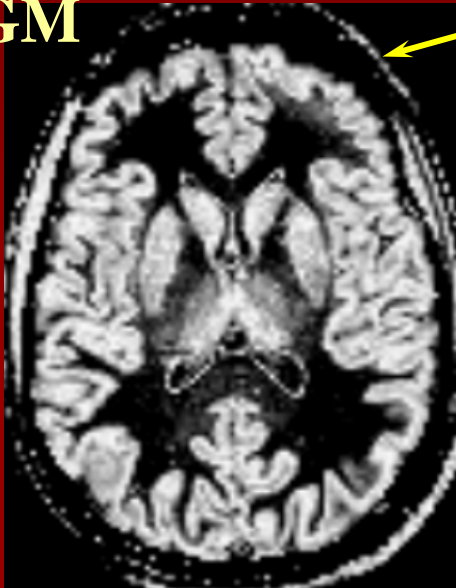
What is ^{13}C MRS?

Image Segmentation

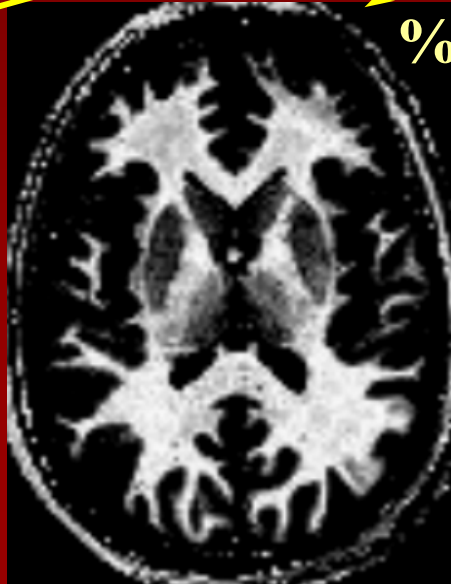
Creating images to quantify
GM, WM, and CSF



%GM



%WM



%CSF

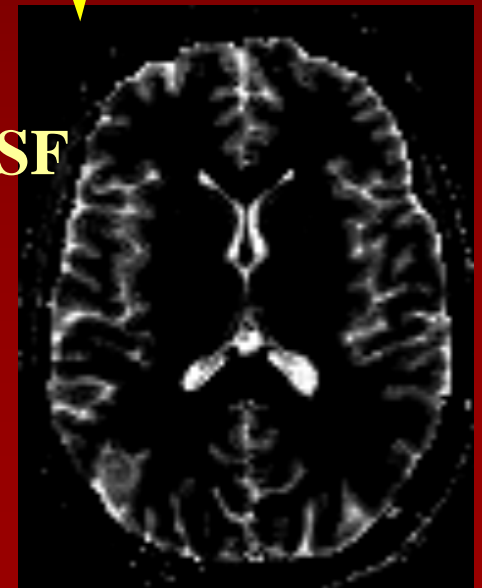
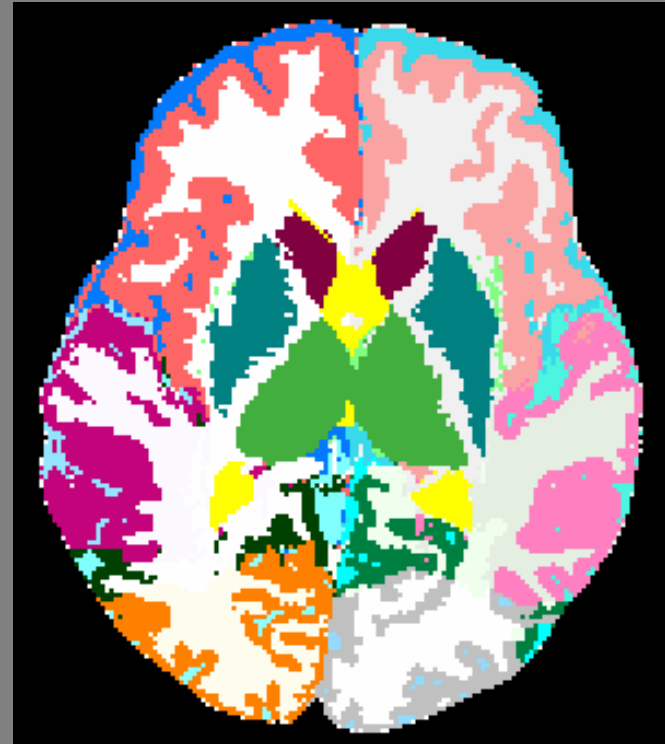
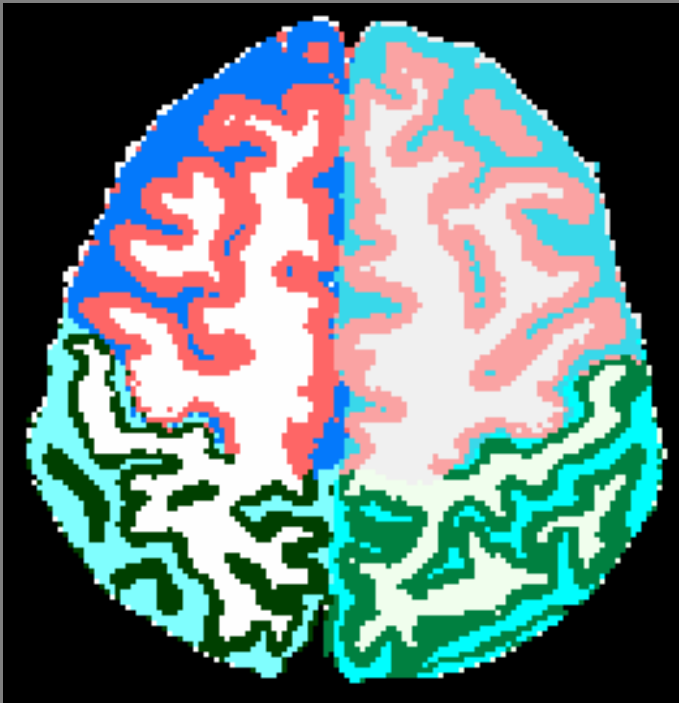
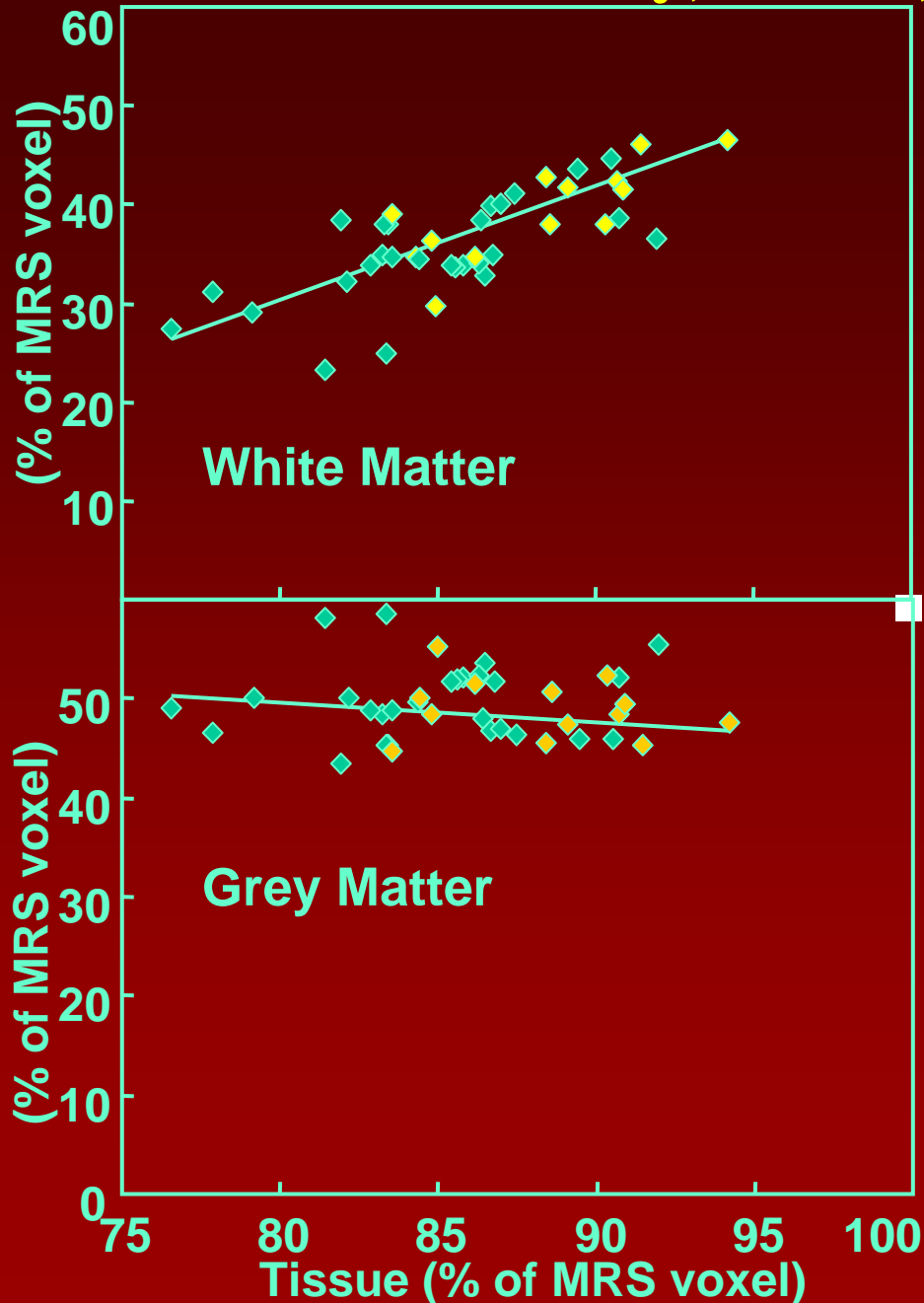


Image Segmentation



Volumes expressed as % of intracranial volume (ICV)

Correlations of Gray, White, and Total Tissue Volumes in Alcoholism

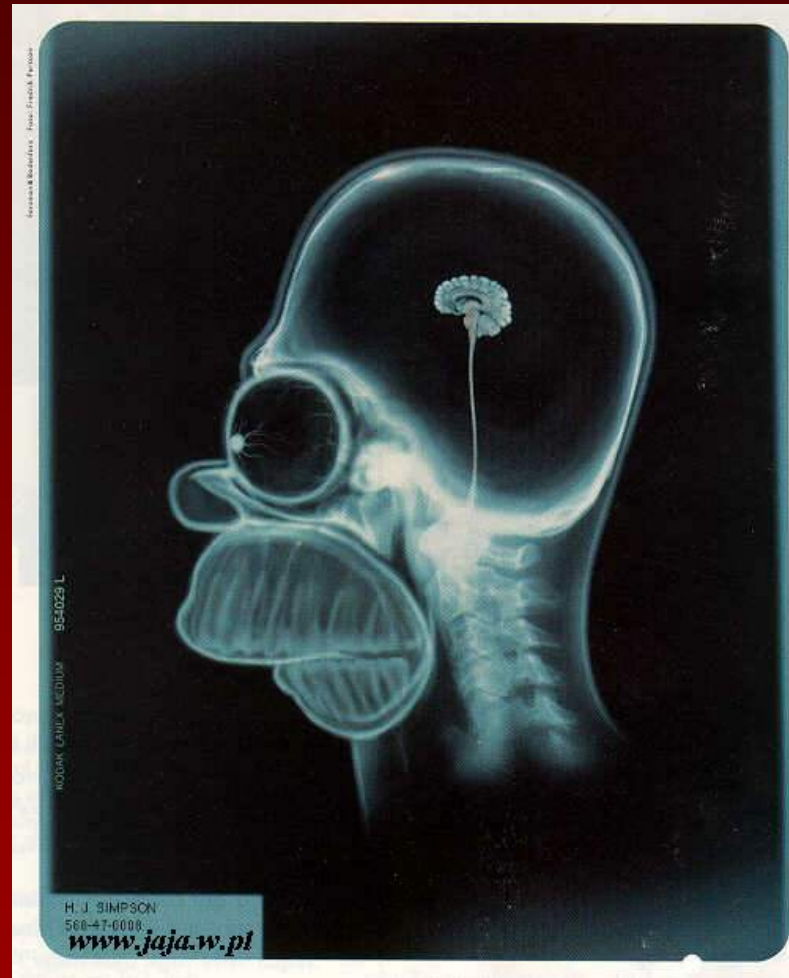


- Across timepoints, there was a significant correlation between white matter content in the voxel and the total solid tissue ($p < 0.0005$), but not between grey matter and solid tissue ($p = 0.36$).

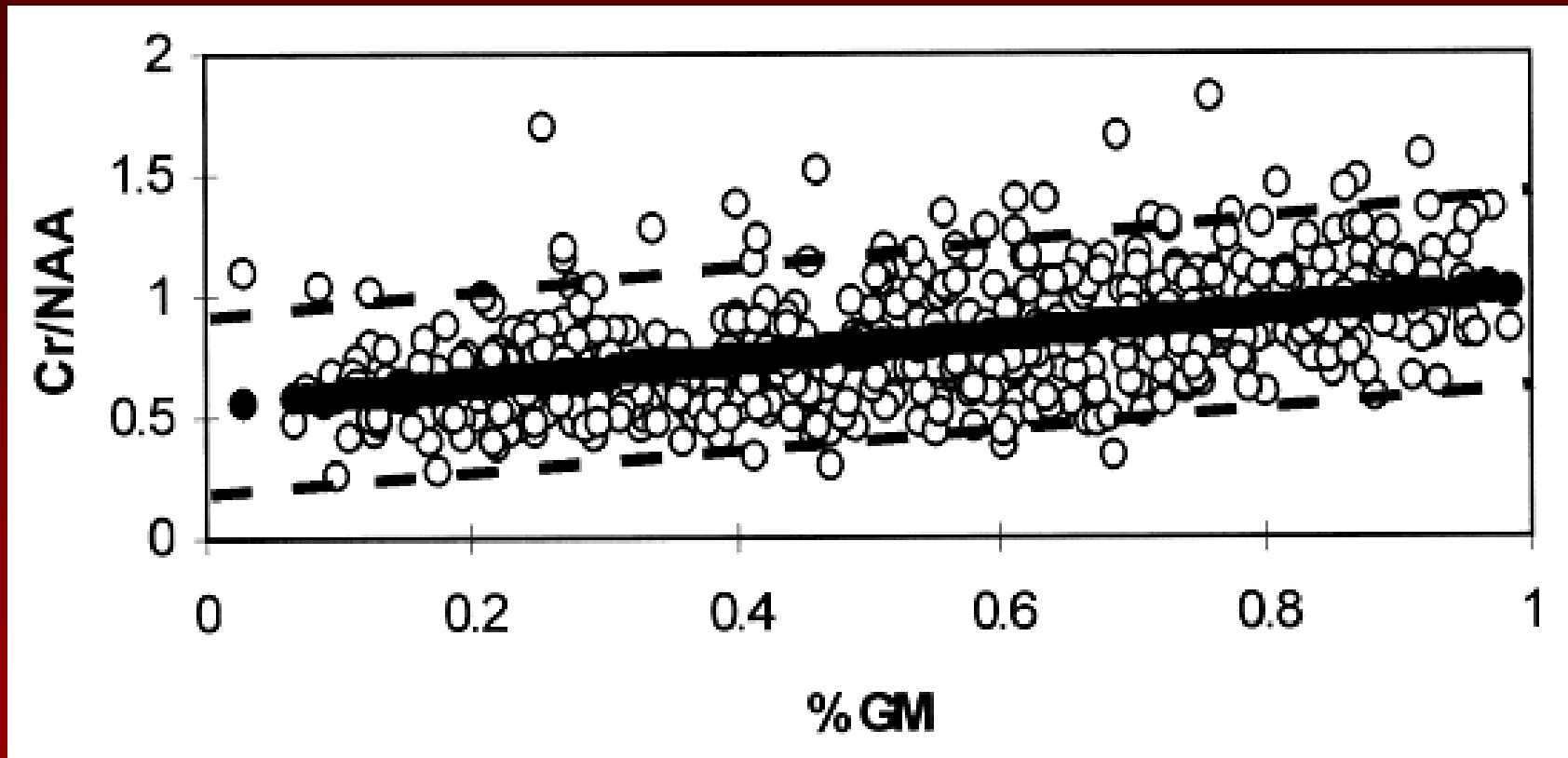
- Significance: long-term improvements in occipital tissue composition are primarily from white matter.

- ◆ Short-term sober subjects
- ◆ Long-term sober subjects

Alcohol-Related Brain Atrophy



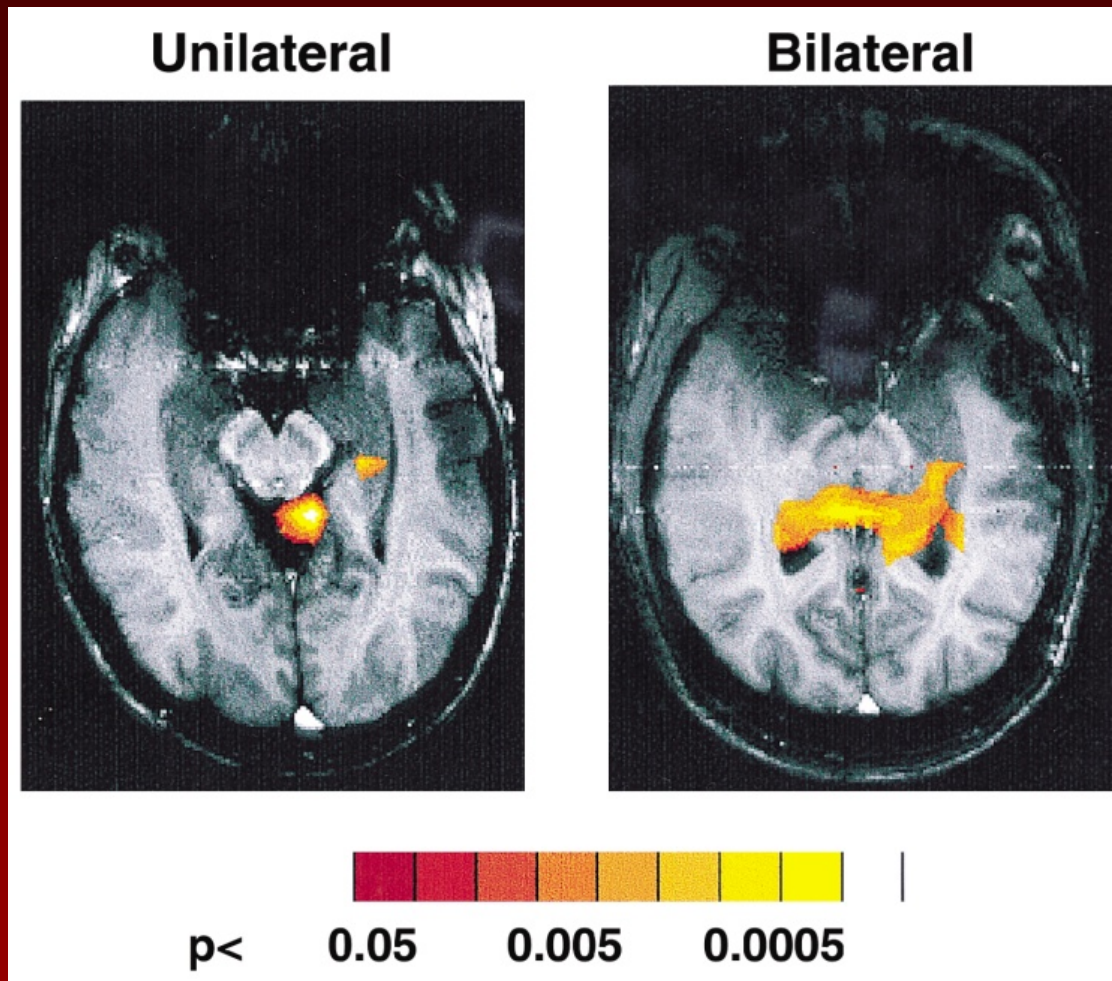
How Can Segmented Data Be Useful?



When pure tissue is not accessible, regression analysis can be used to estimate concentrations in pure tissue.

Chu et al., *Magn Reson Med*, 2000

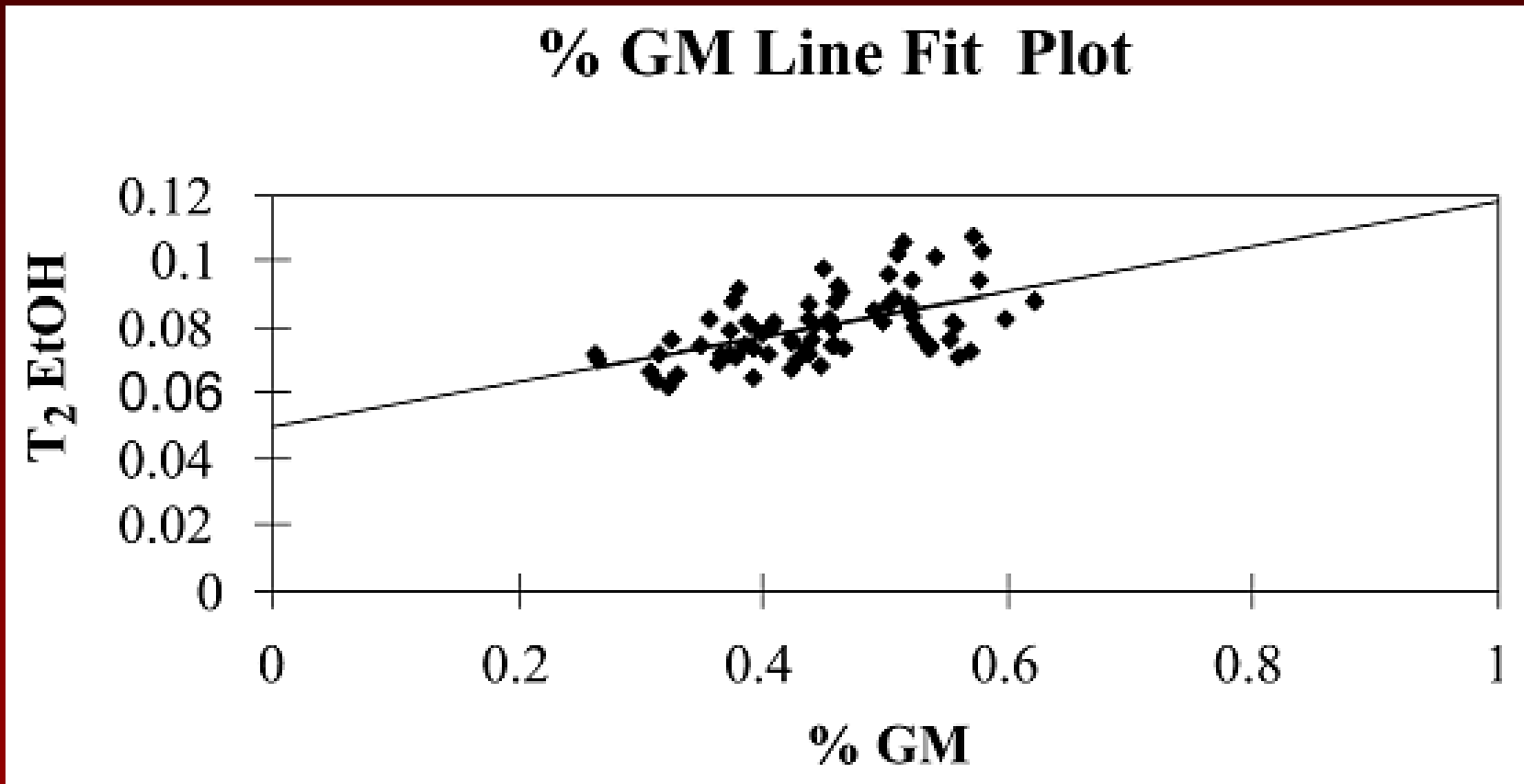
How Can Segmented Data Be Useful?



A disease state can be examined with MRSI and image segmentation. Statistically abnormal pixels can be highlighted.

Chu et al., *Magn Reson Med*, 2000

How Can Segmented Data Be Useful?



When pure tissue is not accessible, regression analysis can be used to estimate T₂ effects in pure tissue.

Sammi et al., Magn Reson Med, 2000

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What is ^{13}C MRS?

^{13}C MRS:

Rates of Metabolism and Neurotransmission, Clear Resolution of Glutamate and Glutamine

- ^{13}C → non-radioactive isotope of carbon.
- 1% natural abundance means low background.
- No isotope effect on metabolism. ■
- Natural labeled substrates in blood yield MRS-detectable products in glutamate, glutamine, and other compounds in the brain.

^{13}C Isotopic Labeling

[4- ^{13}C]Glutamate

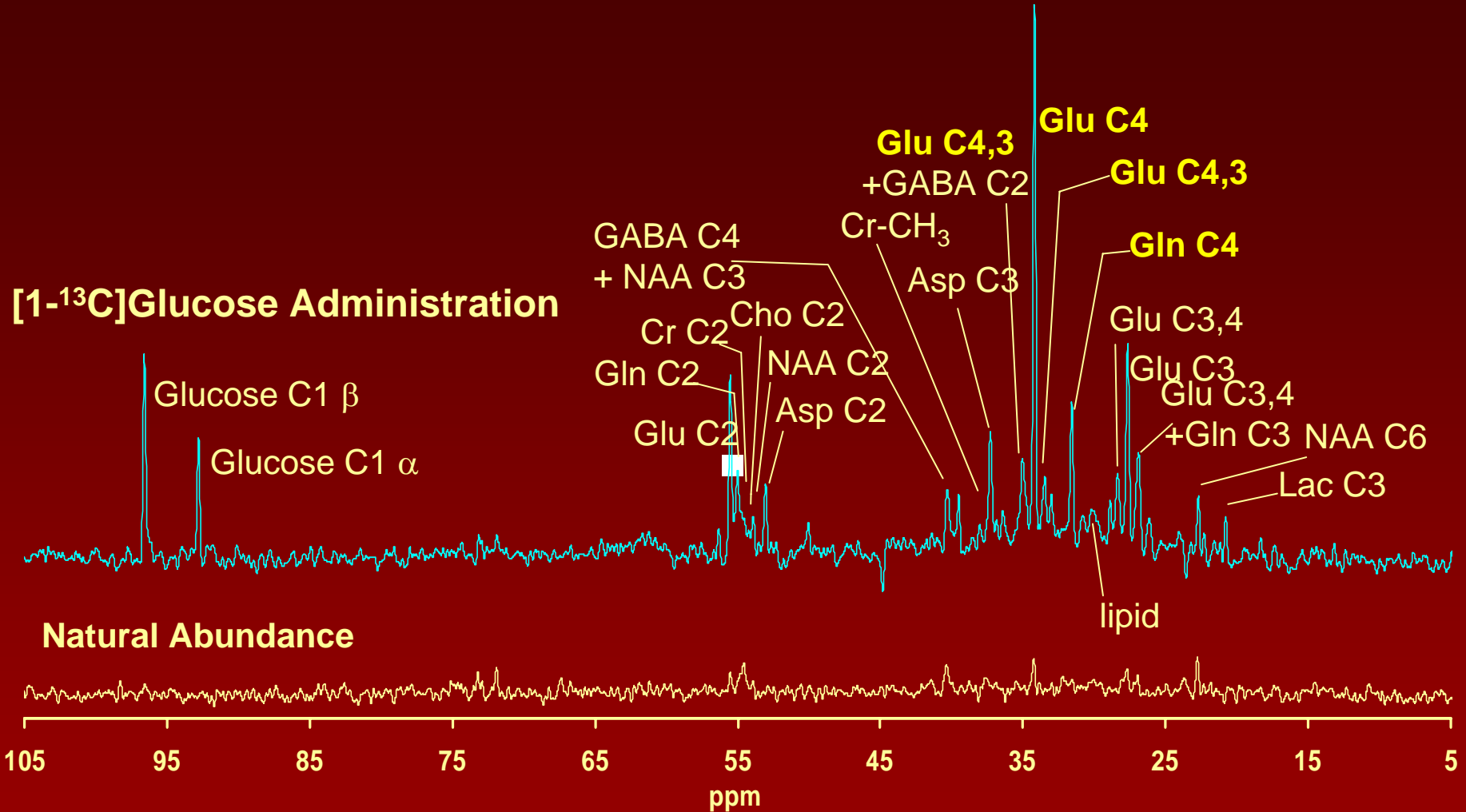
[4- ^{13}C]Glutamine



Time courses of labeling yield rates of metabolic pathways.

[1- ^{13}C]Glucose

A ^{13}C NMR Spectrum of a Human Brain *in Vivo*



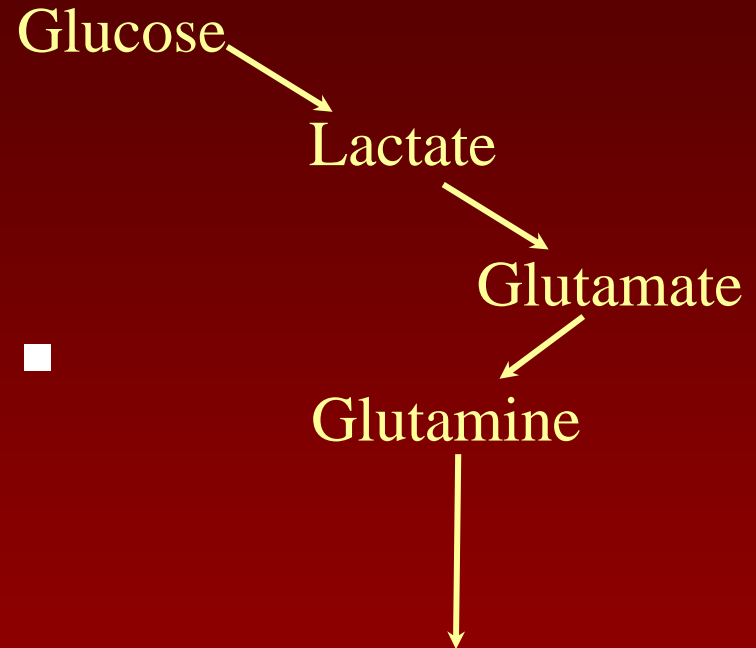
140 cc voxel, 45 min accumulation

Isotopic Flow

Yellow Dye

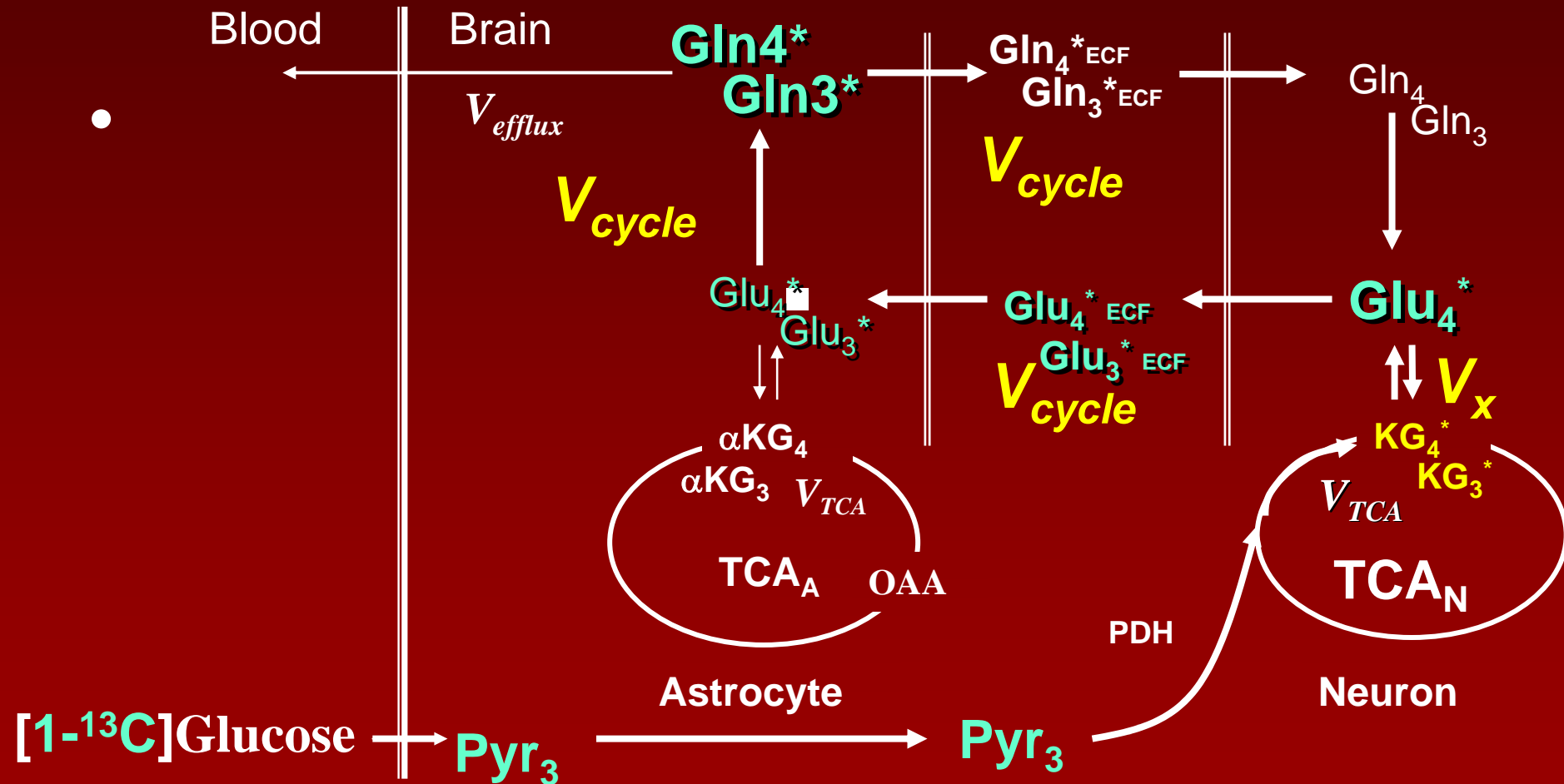


Hana, Maui

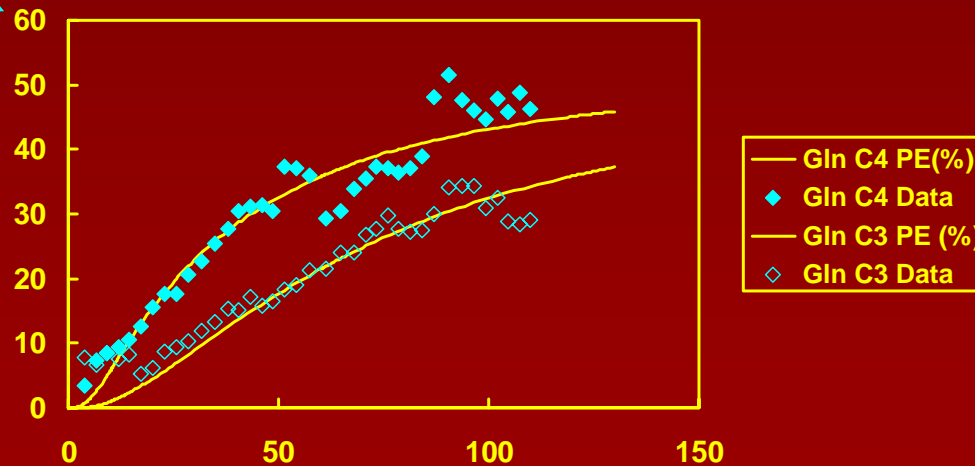
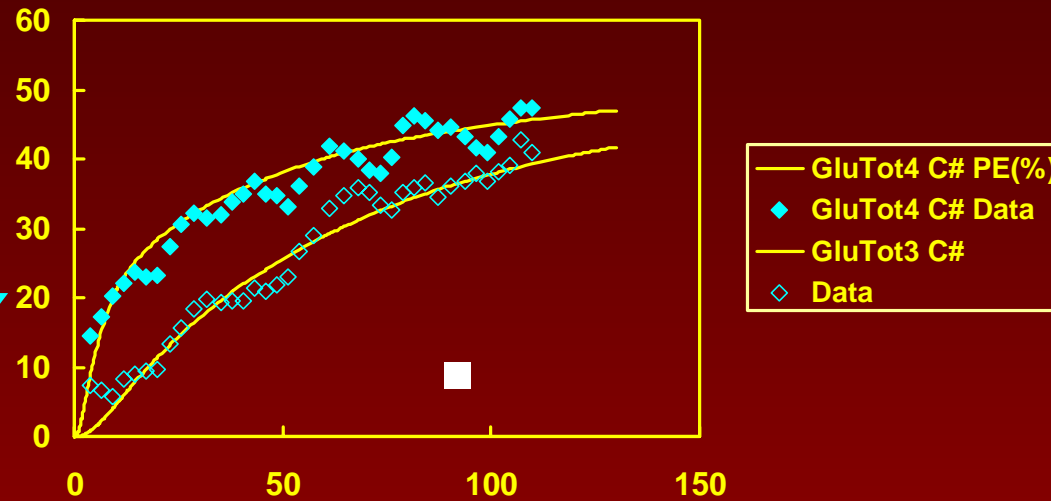


- Faster flow → more rapid appearance of dye at each pool
- Precursor pools “trap” dye temporarily

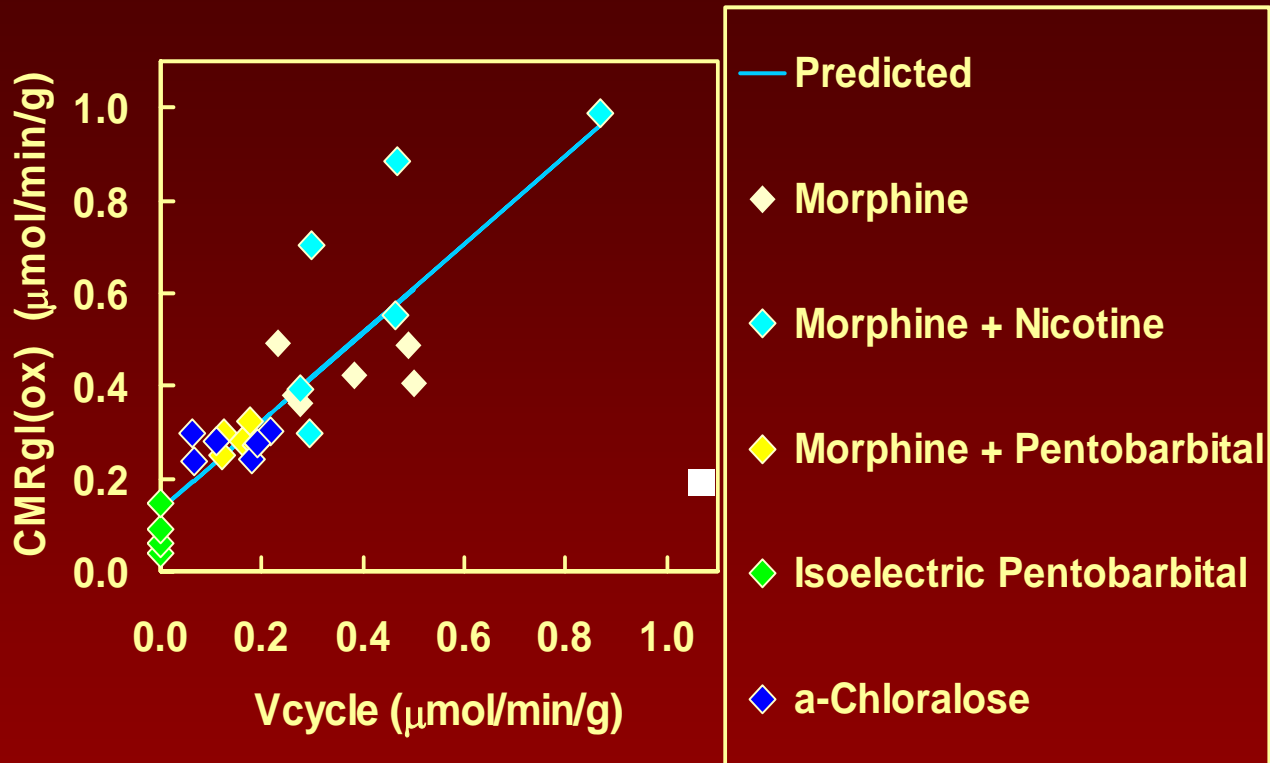
^{13}C Labeling of Neuronal Glutamate & Astroglial Gln by Glutamate/Glutamine Cycle



^{13}C Labeling of Neuronal Glutamate & Astroglial Gln by Glutamate/Glutamine Cycle: V_X , V_{tca} , V_{cycle}



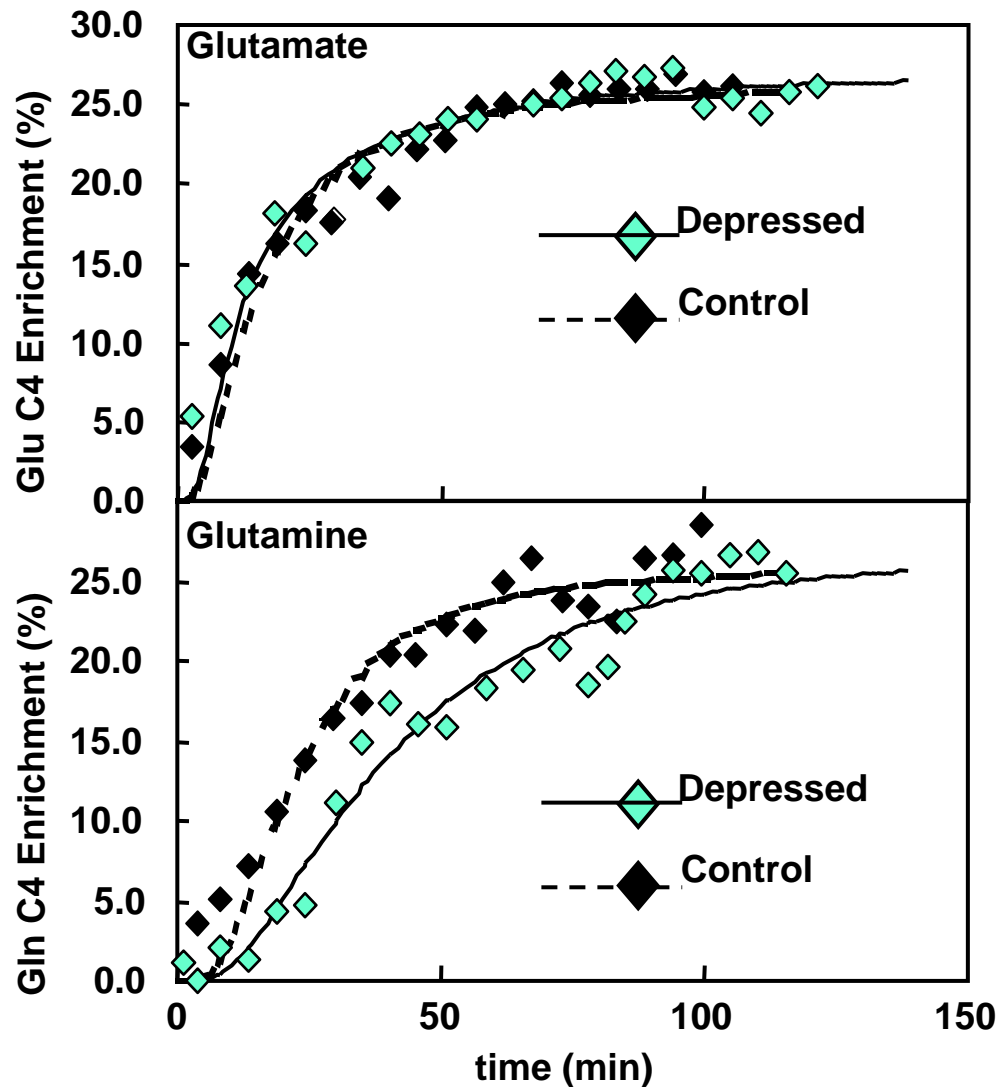
Determining a Relationship Between Glutamate Release and Glucose Oxidation



$$\text{CMRgl(ox)} = 0.13 + 0.96\text{Vcycle}, R^2 = 0.74$$

~1:1 relationship between changes in glucose oxidation and glutamate-glutamine neurotransmitter cycling

^{13}C MR Time Courses of Glu and Gln in Individual Patients and Controls



No difference in oxidative metabolism.

Glutamate-glutamine cycling is reduced in depression.

¹³C MRS Application to Human Disease: Measurement of NAA *Synthesis* in Canavan Disease

Journal of Neurochemistry, 2001, 77, 347–350

RAPID COMMUNICATION

Direct determination of the *N*-acetyl-L-aspartate synthesis rate in the human brain by ¹³C MRS and [1-¹³C]glucose infusion

Angel Moreno,*† Brian D. Ross* and Stefan Blüml*†

*Huntington Medical Research Institutes, Pasadena, California USA

†Rudi Schulte Research Institute, Santa Barbara, California, USA

Abstract

A non-invasive ¹³C magnetic resonance spectroscopy (MRS) technique is described for the determination of the *N*-acetyl-L-aspartate (NAA) synthesis rate, V_{NAA} , in the human brain *in vivo*. In controls, the mean V_{NAA} was 9.2 ± 3.9 nmol/min/g. In Canavan disease, where [NAA] is increased ($p < 0.001$) and [aspartate] is decreased ($p < 0.001$), V_{NAA} was significantly reduced to 3.6 ± 0.1 nmol/min/g ($p < 0.001$). These rates are in close agreement with the activity of the biosynthetic enzyme measured *in vitro* in animals, and with the rate of urinary excretion of NAA in

consistent with the regulation of NAA synthesis by the activity of a single enzyme, L-aspartate-*N*-acetyltransferase, *in vivo*, and with its control in Canavan disease by limited substrate supply and/or product inhibition. The ¹³C MRS technique provides the means for further determination of abnormal rates of neuronal NAA synthesis among neurological disorders in which low cerebral [NAA] has been identified.

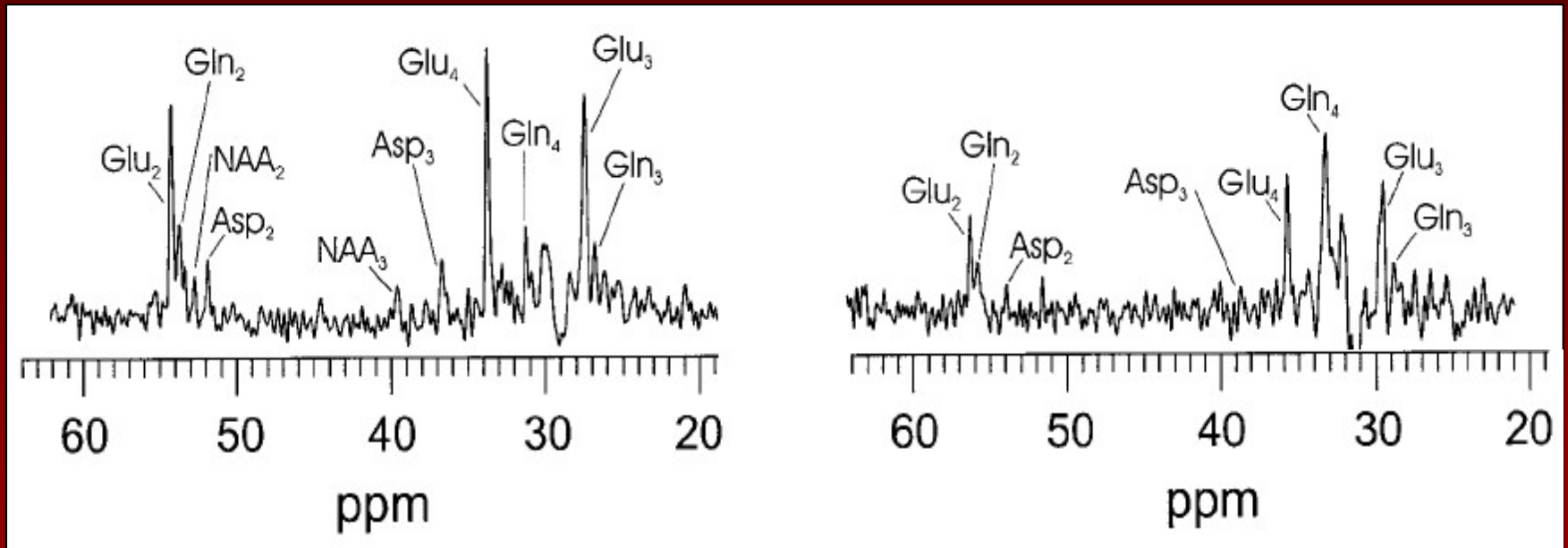
Keywords: ¹³C MRS, [1-¹³C]glucose infusion, Canavan disease, humans, *N*-acetyl-L-aspartate synthesis.

J. Neurochem. (2001) 77, 347–350.

Moreno et al., *J Neurochem*, 2001

¹³C MRS Application to Human Disease

Grading of Hepatic Encephalopathy



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Acknowledgements

Alcohol Studies

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Vladimir Coric

Ralitza Gueorguieva



MRS

Douglas Rothman (MRRC director)

Kevin Behar (GABA expertise, director mouse imaging program)

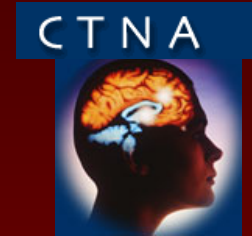
Robin de Graaf

Michael Appel

Nicola Sibson

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Dept. Veterans Affairs**



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Translational Neuroscience
Of Alcoholism**

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K02-AA13430-01**

